

# Pilot Study on the Detection of Simulated Lesions Using a 2D and 3D Digital Full-Field Mammography System with a Newly Developed High Resolution Detector Based on Two Shifts of a-Se

Pilotstudie zur Detektion simulierter Läsionen mit einem 2-D resp. 3-D digitalen Vollfeld-Mammographiesystem und einem neu entwickelten hochauflösenden Detektor auf der Basis von 2 Shifts a-Selens

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## Key words

- breast
- breast tumor
- mammographic density

## Schlüsselwörter

- Mamma
- Mammakarzinom
- mammografische Dichte

## Abstract

**Purpose:** Experimental study of a new system for digital 2D and 3D full-field mammography (FFDM) using a high resolution detector based on two shifts of a-Se.

**Material and Methods:** Images were acquired using the new FFDM system Amulet® (FujiFilm, Tokyo, Japan), an a-Se detector (receptor 24 × 30 cm<sup>2</sup>, pixel size 50 μm, memory depth 12 bit, spatial resolution 10 lp/mm, DQE > 0.50). Integrated in the detector is a new method for data transfer, based on optical switch technology. The object of investigation was the Wisconsin Mammographic Random Phantom, Model 152A (Radiation Measurement Inc., Middleton, WI, USA) and the same parameters and exposure data (Tungsten, 100 mAs, 30 kV) were consistently used. We acquired 3 different pairs of images in the c-c and ml planes (2D) and in the c-c and c-c planes with an angle of 4 degrees (3D). Five radiologists experienced in mammography (experience ranging from 3 months to more than 5 years) analyzed the images (monitoring) which had been randomly encoded (random generator) with regard to the recognition of details such as specks of aluminum oxide (200–740 μm), nylon fibers (0.4–1.6 mm) and round lesions/masses (diameters 5–14 mm), using special linear glasses for 3D visualization, and compared the results.

**Results:** A total of 225 correct positive decisions could be detected: we found 222 (98.7%) correct positive results for 2D and 3D visualization in each case.

**Conclusion:** The results of this phantom study showed the same detection rates for both 2D and 3D imaging using full field digital mammography. Our results must be confirmed in further clinical trials.

## Zusammenfassung

**Ziel:** Experimentelle Studie mit einem System zur Erstellung digitaler 2-D- resp. 3-D-Vollfeld-Mammografien (FFDM) und einem neu entwickelten hochauflösenden Detektor auf der Basis von 2 Shifts a-Selens.

**Material und Methode:** Die Untersuchungen wurden durchgeführt mit dem FFDM-System Amulet® (FujiFilm, Tokio, Japan): a-Se-Detektor (Rezeptor 24 × 30 cm<sup>2</sup>, Pixelgröße 50 μm, Speichertiefe 12 Bit, Auflösung 10 Lp/mm, DQE > 0,50). Integriert in den Detektor ist eine neue Methode des Datentransfers, basierend auf der Optical Switch Technology. Untersuchungsobjekt war das Wisconsin Mammographic Random Phantom, Model 152 A (Radiation Measurement Inc., Middleton, WI, USA). Es bestanden immer gleiche Untersuchungsparameter und Belichtungsdaten (Wolfram, 100 mAs, 30 kV). Wir fertigten 3 unterschiedliche Bilder (Aufnahmepaare) in c-c und ml Ebene (2-D) resp. in c-c und c-c Ebene mit einem Winkel von plus 4° (3-D) an. Fünf in der Mammografie erfahrene Radiologen (3 Monate bis mehr als 5 Jahre) werteten die zufallsverteilten Bilder (Monitoring) in Hinblick auf die Detektion von Aluminiumoxidpartikeln (200–740 μm), Nylonfäden (0,4–1,6 mm) und Rundherden (Durchmesser 5–14 mm), wobei zur 3-D-Visualisierung eine lineare Polfilterbrille (3-D) verwendet wurde, aus und verglichen die Ergebnisse.

**Ergebnisse:** 225 richtig positive Entscheidungen waren möglich: Wir fanden für die 2-D- und 3-D-Visualisierung jeweils 222 (98,7%) richtig positive Ergebnisse.

**Schlussfolgerung:** Die Ergebnisse dieser Phantomstudie demonstrieren sowohl für die 2-D- als auch 3-D-Bildgebung in der digitalen Vollfeld-Mammografie gleiche Entdeckungsraten. Weitere klinische Studien sind hierzu notwendig.

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## Introduction

The development of digital image receptor systems in mammography has progressed to such an extent over the past few years that, in addition to their conventional application, digital mammography systems can now also be used as a platform for further, new examination methods such as contrast mammography or tomosynthesis [1–6].

Digital breast tomosynthesis (DBT) has the potential to remove undesirable masking as a result of superimposed layers and thus reduces false-positive or false-negative examination findings. Whether DBT can be regarded as an alternative to digital mammography or whether it is just an additional examination method in assessment diagnostics is as yet not clear [7–14].

A novel method comprising 2 stereo mammography images (stereoscopy) (● Fig. 3) using linearly polarised filter glasses produces a 3-dimensional (3D) overall image (visualisation) of the breast.

The aim of the pilot study was to examine the detection of simulated mammographic lesions (micro-calcifications and tumour-like masses) with these novel mammography methods and to contrast these with the findings from another, already established mammography system.

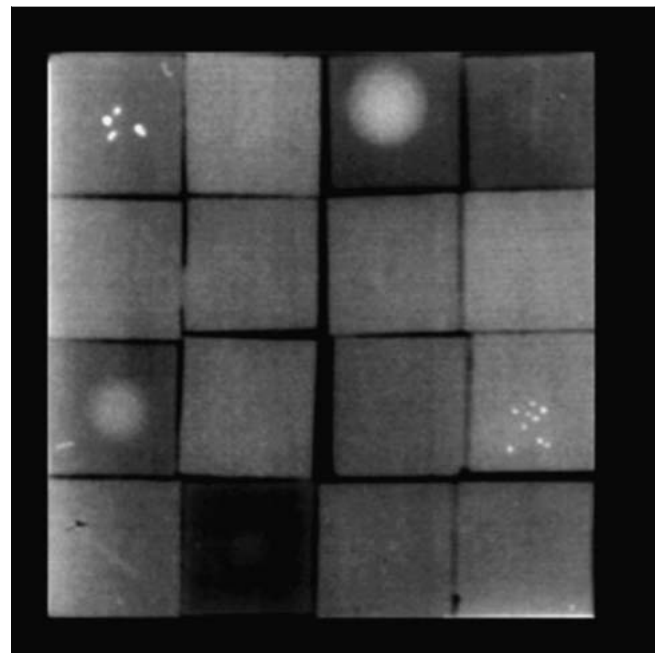
## Material and Method

For the examinations the Amulet digital mammography system (FujiFilm, Tokyo, Japan) was used. This system operates with a  $24 \times 30 \text{ cm}^2$  detector which is firmly integrated into the system [15,16]. This totally novel detector is constructed from two superimposed layers of high-purity amorphous selenium, separated by a very thin layer of selenium that is just  $1 \mu\text{m}$  thick and has been doped in a targeted manner with foreign atoms. This detector achieves a pixel size of  $50 \mu\text{m}^2$ .

The mammography system is fitted with a bimetal x-ray tube, which offers the options of molybdenum or tungsten as anode material in combination with molybdenum or rhodium filters. Within the scope of the present investigation all images were made with a manually set molybdenum/molybdenum combination and an x-ray current-time product of 100 mAs at a tube voltage of 30 kV (● Table 1).

We initially took 3 different images (image pairs) in c-c and ml views (2D) and in the c-c view and c-c view with an angle of plus  $4^\circ$  (stereoscopy), respectively.

As in earlier studies [17] the Wisconsin Mammographic Random Phantom (Model 152 A, Gammex Inc.) was selected as test object



**Fig. 1** Wisconsin RMI Phantom, Model 152 A, Radiation Measurements, Middleton, WI, USA. 16 wax blocks with 4 round lumps, 5 calcifications, 6 threads, 1 empty, raised radiolucent position 4.5 cm, net density 1.5.

(● Fig. 1). This phantom contains a total of 5 elements with micro-calcifications, 6 with thread-like structures and 4 with tumour-like masses. These 15 simulated lesions are located in 15 separate wax blocks in the phantom; in addition one empty wax block without lesions is present. The wax blocks are interchangeable, so that different distribution patterns in the phantom can be realised. A learning effect can thus be avoided for the evaluators. The complete phantom recreates a standard breast with a compression layer thickness of approx. 4.5 to 5 cm.

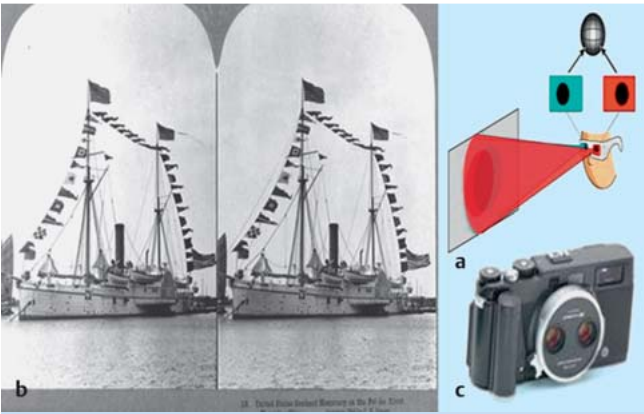
The evaluation of the phantom image was performed on a  $2.5 \times 2.5 \text{ k}$  monitor by five radiologists with varying years of mammographic experience. Each radiologist was shown 3 image pairs (images in c-c and ml views) (2D) with different phantom compositions and in the c-c view and c-c view with an angle of plus  $4^\circ$ , respectively, using linearly polarised glasses (3D) for evaluation. In linearly polarised filter glasses the light is polarised linearly, i.e. the light oscillates within a plane determined by the filter. Here the filters must be positioned at a right angle to one another for the left and right viewing position in order to enable the separation of the two views and to achieve a 3D visualisation (● Figs. 2 and 3). The viewing time per image was limited to a maximum of 5 minutes. As part of the study the detection sensitivity with the new mammography method was to be evaluated – for this reason the correct positive rate for each individual lesion type was determined.

## Findings

● Table 2 lists the findings of the study determined by the 5 evaluators, broken down according to the digital mammography system used, the different examination methods (2D and 3D respectively) and the lesion type. Additionally, the number of lesions actually present and the resulting detection rate, as well as the

**Table 1** Parameters of the mammography system during examination.

	Amulet
Manufacturer	FujiFilm
Anode	Mo, W
Filter	Mo, Rh
Scattered radiation grid	linear
Conversion material	Semiconductor a-Se
Sampling process	Optically induced sampling
Pixel size	$50 \mu\text{m}$
Spatial resolution (Nyquist Frequency)	10 lp/mm
Field size	$24 \times 30 \text{ cm}^2$



**Fig. 2 a to c** Stereoscopy. The distance between the human eyes is roughly 65 mm, i.e. each eye has a different view of the three-dimensional world. Through these 2 different viewpoints of a virtual system we are able to determine the relative depth of different objects in the object viewed, because the 2 independent images are combined within the brain to determine the depth (a and b). This process is used in photography by making 2 standard images (0° and 4° projection) in order to simulate natural sight (c).

mean finding determined on the basis of the three lesion types, are given.

With the digital mammography system and the dual layer selenium detector a detection rate of 97.7% was computed both for each of the 3 image pairs (images in the c-c and ml views) (2D) with differing phantom composition and the 3 image pairs in the c-c view and c-c plane with an angle of plus 4° (stereoscopy), respectively, using linearly polarised filter glasses for visualisation (3D).

**Discussion**

The most important image-producing method for the early diagnosis of breast cancer remains x-ray mammography. It is the only method with proven use as a quality-assured screening method to lower the breast cancer mortality rate. Full-field digital mammography, or FFD, is today regarded as the standard mammographic method, both in curative mammography and in the preventive mammographic screening of women without any symptoms and, in particular, is more effective for the detection of pathological findings in women with dense breasts than standard film foil mammography [1–6]. Nonetheless, as with all radiological projection methods, digital mammography suffers from the fact that it depicts three-dimensional information as a two-



**Fig. 3 a to c** 3D digital full field mammography. Monitoring with mammographies in the c-c view and c-c view with an angle of plus 4° (stereoscopy), respectively (a and b) with the use of linearly polarised filter glasses in order to obtain a holistic 3D image of the breast (c).

dimensional image. Superimposed structures are projected onto one image plane, so that lesions of clinical relevance can easily be covered and their viewing obstructed by overlapping tissue. This increases the frequency of false-negative examination findings, i.e. existing carcinomas are overlooked. Such overlapping of normal breast tissue may also result in false-positive examination results, in that they mock malign lesions which then lead to the patient having to undergo an unnecessary repeat examination and may even result in an unnecessary biopsy.

The development of digital image receptor systems in mammography has progressed to such an extent over the past few years that, in addition to their conventional application, digital mammography systems can now also be used as a platform for further, new examination methods such as contrast mammography or tomosynthesis. Digital breast tomosynthesis, or DBT, is an imaging technology which can deliver layered images free from overlaps on the basis of a limited number of individual images taken at different projection angles. The exposure parameters for each individual layer are selected in such a way that the radiation exposure resulting from all images taken is preferably lower than the radiation dose from a 2-plane mammography. With the aid of different reconstruction algorithms the breast is subsequently visualised in the layers of interest at various depths parallel to the detector surface.

Digital breast tomosynthesis has the potential to remove undesirable masking as a result of superimposed layers and thus reduces

**Table 2** Number of correctly detected simulated lesions using the digital mammography system and the detection rate in per cent averaged over the five evaluators, each three phantom configurations (c-c and ml plane [2D] and c-c and c-c plus 4° plane, respectively [3D]).

	Amulet c-c and oblique plane 2D	Amulet c-c and c-c plus 4° plane 3D	Really existing lesions
Threads	18.0 (100%)	18.0 (100%)	18
Microcalcifications	14.3 (95.6%)	14.3 (95.6%)	15
Tumour-like masses	12.0 (100%)	12.0 (100%)	12
All lesions	44.4 (98.7%)	44.4 (98.7%)	45



false-positive or false-negative examination findings. Whether DBT can be regarded as an alternative to digital mammography or whether it is just an additional examination method in assessment diagnostics is as yet not clear [7–14].

A novel method on the basis of 2 mammography images (c-c and c-c plus 4°) (stereoscopy) (● Fig. 2) has been developed in order to obtain a three-dimensional overall image of the breast (3D) (● Fig. 3) with the use of linearly polarised filter glasses.

The present study is the first phantom study based on a digital mammography system (● Table 1) to compare the detection of simulated microcalcifications, thread-like structures and tumour-like masses in 2D and 3D visualisation (● Fig. 1) [15, 16]. The detected findings listed in ● Table 2 do not, however, show any differences. While the simulated microcalcifications could be detected with an efficiency of up to 95.6% with both visualisation methods – 100% of the thread-like structures and tumour-type masses were detected. This shows that the phantom used is at least sufficient for a rough orientation, but is not sufficient for a differentiated evaluation of powerful digital imaging systems. This is also confirmed by the fact that, in terms of the phantom examination, no great differences in the detection rates occurred despite the great discrepancy in experience between the 5 evaluators (from 3 months to 5 years).

Despite all limitations, the present findings with the Wisconsin Mammographic Random Phantom (● Fig. 1) [17] must be evaluated as meeting all necessary minimum requirements. They cannot furnish an adequate basis for unlimited clinical application of the new system. Such conclusive findings could only be furnished by a comprehensive study on the contrast resolution capability with the currently valid national and international standard phantom CDMAM Phantom [18, 19]. However, even with this test specimen, disregarding any anatomical noise only objects in front of a homogenous background can be detected. Furthermore, newly developed phantom systems exist [20, 21], the final findings of which are yet to be determined.

The new method for the three-dimensional representation of the breast in one holistic image with the use of linearly polarised filter glasses represents an important innovation, in particular in comparison with tomosynthesis [22]. In addition, at the same time it is the deciding step towards a real, so to speak, online 3D visualisation of the breast in future made available at any desired workplace (PACS). To this end, besides the respective software, monitors with a resolution of at least 3.5 × 3.5 k are necessary, making additional aids (e.g. glasses) obsolete. Developments in this respect are still in the experimental stage. Whether an improvement in the detection rate of examination findings to be clarified (correct positive findings) while at the same time reducing false-negative findings – also by using computer-aided diagnostic systems (CAD) – can actually be achieved, remains to be seen. However, the prospect of real 3D-controlled intervention and planning oncology management, including plastic surgery, appears to be promising.

## Conflict of Interest

▼  
None.

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