

Use of 3D Navigation in Subaxial Cervical Spine Lateral Mass Screw Insertion

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Abstract

Objective Cervical spine can be stabilized by different techniques. One of the common techniques used is the lateral mass screws (LMSs), which can be inserted either by freehand techniques or three-dimensional (3D) navigation system. The purpose of this study is to evaluate the difference between the 3D navigation system and the freehand technique for cervical spine LMS placement in terms of complications. Including intraoperative complications (vertebral artery injury [VAI], nerve root injury [NRI], spinal cord injury [SCI], lateral mass fracture [LMF]) and postoperative complications (screw malposition, screw complications).

Methods Patients who had LMS fixation for their subaxial cervical spine from January 2014 to April 2015 at the Ottawa Hospital were included. A total of 284 subaxial cervical LMS were inserted in 40 consecutive patients. Surgical indications were cervical myelopathy and fractures. The screws' size was 3.5 mm in diameter and 8 to 16 mm in length. During the insertion of the subaxial cervical LMS, the 3D navigation system was used for 20 patients, and the freehand technique was used for the remaining 20 patients. We reviewed the charts, X-rays, computed tomography (CT) scans, and follow-up notes for all the patients pre- and postoperatively.

Results Postoperative assessment showed that the incidence of VAI, SCI, and NRI were the same between the two groups. The CT scan analysis showed that the screw breakage, screw pull-outs, and screw loosening were the same between the two groups. LMF was less in the 3D navigation group but statistically insignificant. Screw malposition was less in the 3D navigation group compared with the freehand group and was statistically significant. The hospital stay, operative time, and blood loss were statistically insignificant between the two groups.

Conclusions The use of CT-based navigation in LMS insertion decreased the rate of screw malpositions as compared with the freehand technique. Further investigations and trials will determine the effect of malpositions on the c-spine biomechanics. The use of navigation in LMS insertion did not show a significant difference in VAI, LMF, SCI, or NRI as compared with the freehand technique.

Keywords

- freehand
- lateral mass screw
- 3D navigation
- cervical spine
- subaxial spine
- fixation complication

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Introduction

Different techniques have been used for posterior stabilization of the cervical spine; some of these techniques include interlaminar wiring, lateral mass screw (LMS), and pedicle screws.¹ LMS fixation is one of the common techniques used for treating unstable cervical spine due to different pathologies such as trauma, rheumatoid arthritis, tumors, osteoarthritis, etc. Compared with other cervical spine stabilization techniques, LMS fixation has been proven to be effective and safe.¹ This technique requires a posterior cervical approach with a dissection through the paraspinal muscles. In addition, bony landmarks have to be outlined prior to any LMS instrumentation.

Polyaxial screws have enabled angulated trajectories for placing longer screws toward the superior-lateral-ventral corner of the lateral mass.² In addition, the improvement in LMS constructs, from posterior cervical plating to rod-based systems, has provided additional advantages such as greater amenability to multiplanar contouring, increased flexibility for extending to the occiput or the thoracic spine, and more precise screw placement.²

Roy-Camille et al was the first to insert an LMS in the cervical spine in 1979.^{2,3}

In the following years, LMS instrumentation has been described and modified by various researchers.^{1,4–6} Each of these techniques has a different entry point and trajectory in the sagittal and axial planes. In 2008, Ching⁷ used a modified Magerl's technique and reported good results and low complication rate. With the different available techniques for LMS insertion, the malposition of these screws can lead to complications. LMS complications can be divided into intraoperative complications (vertebral artery injury [VAI], nerve root injury [NRI], spinal cord injury [SCI], lateral mass fracture [LMF]) and postoperative complications (screw malposition, screw complications like pullout, breakage, or loosening).¹

The use of three-dimensional (3D) navigation in spine surgery allows the surgeon to navigate the patient's spine by loading a computed tomography (CT) scan to the system preoperatively.⁸ The navigation technology has advanced greatly due to the high speed computers that integrate the navigation data.⁹ The navigation systems can be based on intraoperative two-dimensional (2D)/3D fluoroscopy, CT scan, or magnetic resonance imaging (MRI). The CT-based navigation systems help the spine surgeons to accurately place spinal instrumentation (pedicle screws, LMS, and interbody fusions). The use of either a preoperative CT scan or an intraoperative 3D fluoroscopy-based navigation has the advantage of outlining the bony landmarks compared with the MRI. Registration in the navigation system can be either single-time multilevel registration or the level-by-level registration method.¹⁰ Registration can be by paired points (3–4 points), surface matching technique, or combined combination of techniques. Checking the accuracy of the navigation at each level before instrumentation is an important indicator for possible reregistration.

The aim of this study is to evaluate the different complications associated with the LMS for the cervical spine fixation screw malposition and compare the 3D navigation group with the freehand group.

Methods

Study Population

We retrospectively studied 40 patients with LMS instrumentation from January 2014 to April 2015 at the Ottawa Hospital. All the included patients had cervical instrumentation with LMS; the 3D navigation technique was used in 20 patients, and the freehand technique was used for the other 20 patients. We studied the LMS in the subaxial spine from C3 to C7.

The inclusion criteria were age 18 years and above, fracture of the subaxial cervical spine or cervical degenerative disc disease associated with myelopathy as an indication, at least 1 level of LMS fixation (2 vertebrae) from C3 to C7, and patients with extension of instrumentation to occiput or the thoracic spine. The exclusion criteria were patients who had previous cervical instrumentation or patients who had 4 mm diameter LMS.

Surgical Technique for 3D Navigation Group

In this group, all surgeries were done under general anesthesia. We used CT scan-based navigation, and the images were uploaded to the Stryker navigation system preoperatively. Both the Stryker navigation probe and the array used in the procedures have three spheres. The patients were operated on the prone position, and their heads were fixed to the Mayfield frame. Preoperative antibiotic was also administered. Our approach was midline posterior with subperiosteal paraspinal muscle dissection to the lateral edge of the lateral masses. We identified the levels using a cross-table 10-ray and hooked the navigation array to either the distal or proximal exposed spinous processes. Then, we started the registration using the combined technique, which included paired points (4–5 points) with an acceptable accuracy of < 2 mm, followed by surface match technique—~30 points—to increase the accuracy.¹¹ We accepted an error of up to 2 mm in accuracy; in the case of a larger error, reregistration was considered. The pair point and the surface match techniques were performed on two consecutive vertebrae. The posterior elements of each. We used a single-time multilevel registration and checked our accuracy at each level using the spinous process and the facet joint as a mark to decrease the operative time (→ Fig. 1).

We started our fixation using a matchstick drill to create the pilot holes. Then, we used either the power drill or the manual drill to create the lateral mass holes, aiming our LMS trajectory to be in the superior lateral quadrant. We used either the Oasys system from Stryker or the Synapse system from DePuy Synthes. The sizes of the used LMS were 3.5 mm × 8 to 16 mm.

Surgical Technique for the Freehand Group

The above preparation was also followed in this group. We used the modified Magerl's (Ching) technique for cervical spine LMS insertion, in which the entry point was 1.5 mm caudal and medial to the center of the lateral mass and had a relatively more oblique (30°–40°) and steeper (35°–45°) trajectory, aiming our LMS trajectory to be in the superior lateral quadrant (Zone 1) (→ Fig. 2).

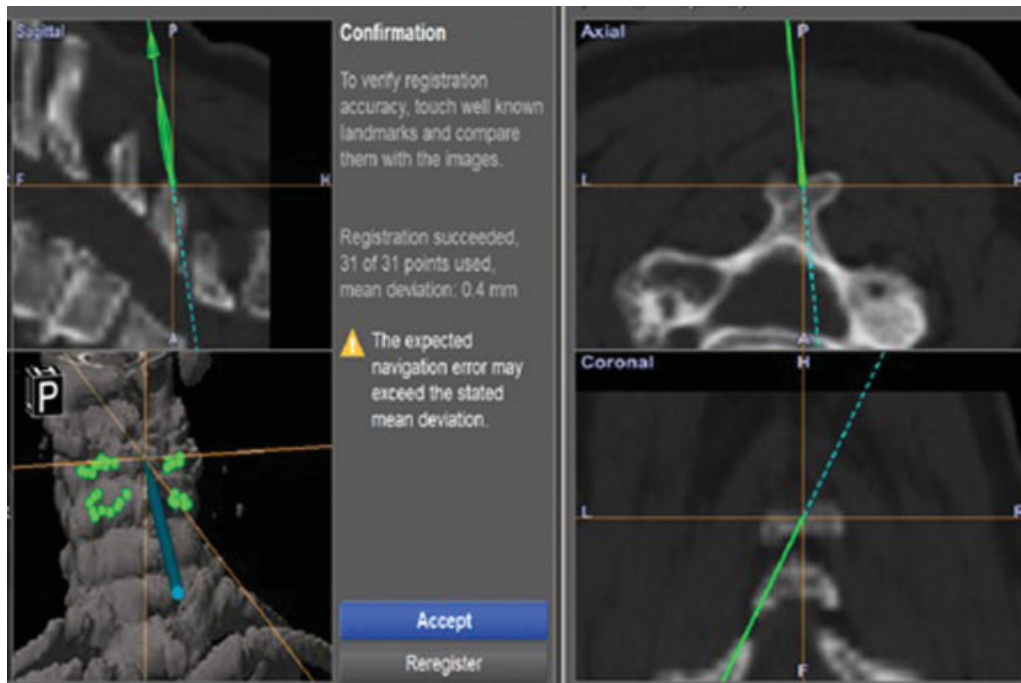


Fig. 1 (A) The surface match registration and (B) confirming registration.

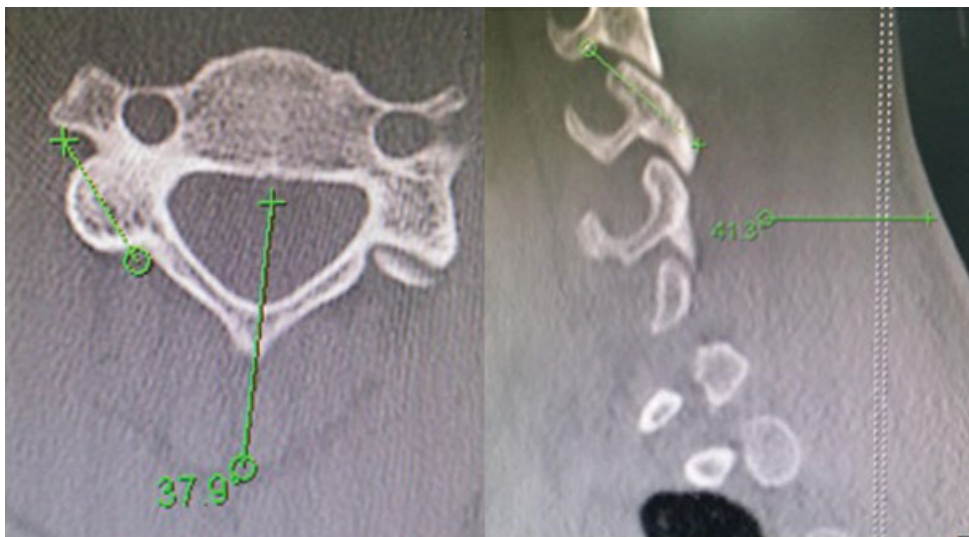


Fig. 2 (A) Axial trajectory. (B) Vertical trajectory.

Follow-Up Assessment

The patients in both the groups wore a Philadelphia collar for 3 months. All the patients had postoperative serial X-rays and clinical assessment immediately after surgery, and at 3, 6, and 12 months' follow-up. All the patients also had cervical spine CT scans 6 weeks after the surgery. The mean follow-up duration was 13 months.

Clinical Assessment

For clinical assessment, we addressed intraoperative VAI by heavy bleeding¹² and SCI and NRI by the cerebrospinal fluid leak associated with postoperative neurological deficit. LMF was assessed intraoperatively by any crack induced in the

lateral mass while performing the fixation.¹ The development of any symptoms or signs indicating neurovascular injuries (VIA, SCI, NRI) such as sensory or motor deficits and visual impairment were reviewed from the patient's chart.¹

CT Scan Assessment

CT scans were done using 2.5 mm thickness cuts. The sagittal and axial cuts were assessed by the independent interobserver, who did not contribute to any of the surgeries. The spatial relationship between the screw and the foramen transversarium (FT) was evaluated on axial plane CT images based on the location of the screw tip in relation to the edge of the vertebral artery (VA) foramen.¹

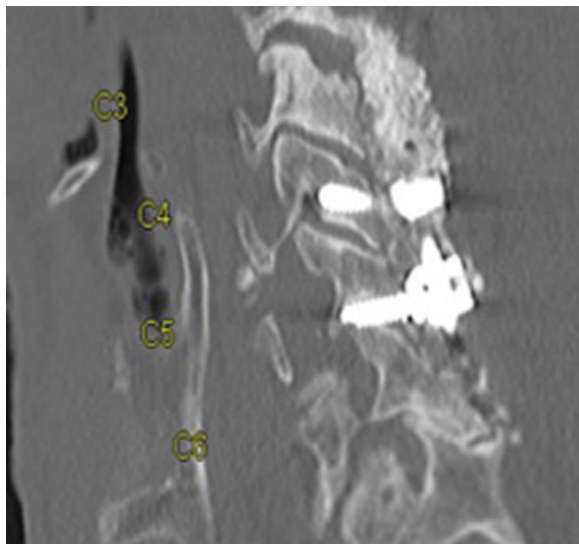


Fig. 3 Screws at Zones 2 and 3 according to Heller's classification in C4 and C5.

"The zones for the tip of the screw are defined by Heller et al as follows: Zone 1 is the superior margin of the superior articular process, Zone 2 includes the ventral portion of the lateral mass that forms the roof of the neuroforamen and the transverse process that protects the nerve root as it exits the neuroforamen, and Zone 3 extends from the inferior origin of the transverse process to the tip of the inferior articular process."^{13,14} We defined the screws with breaching tips at Zones 2 and 3 as malpositioned, see ► **Fig. 3**.

Statistical Analysis

The following data were collected: demographic data (age, sex, etc.), indication for surgical intervention, date of surgery, number of cervical spine levels that were instrumented, number of LMSs at each level, intraoperative events (VAI, LMF, and neurologic injury), use of intraoperative 3D neuronavigation, and cervical spine alignment (postop day 1, 3, 6, and 12 months' follow-up). The data were stratified into two groups: group 1 patients had their surgery using the freehand technique, and group 2 patients had their surgery using 3D navigation. The analysis was done by comparing the primary outcome, which is screw malposition, and secondary outcome that includes the number of LMS, hospital stay, cervicothoracic/occipitocervical extension, and blood loss between the two groups.

For each subject, the malpositioned screws were collected for each patient (e.g., 0, 1, 2...). We calculated the percentage of screw malposition among the total number of LMS for each patient. The total number of LMS for each patient was considered as a weighted variable. The weighted arithmetic means and the weighted standard deviation (SD) of the percentage of malpositioned screws were also calculated.

The weighted mean was defined as $\bar{x}_w = \frac{\sum_i w_i x_i}{\sum_i w_i}$, the weighted variance was defined as $s_w^2 = \frac{1}{d} \sum_i w_i (x_i - \bar{x}_w)^2$, where w_i is the weight for the i th subject, x_i is the i th variable value, and the divisor d is $n - 1$. The weighted variance is a measure of variability, and it is the sum of the weighted squared distance

of data value from the mean divided by the variance divisor, which is defined to be $n - 1$.

We calculated the mean, range, and median (95% confidence interval [CI]) for each group demographic data, ratio of intraoperative events for each group, the ratio of misalignment within each group, and ratio of implant failure within each group. The two groups were compared using t -test (for continuous variables) and chi-square test (for binomial variables and ratios). We also conducted multivariable analysis for the primary outcome within each group and compared the ratio of the primary outcome between the two groups. We conducted the statistical analysis using the α of 0.05 using Excel and Statistical Analysis Software (SAS).

To compare the difference between these two treatment groups, we applied Wilcoxon rank-sum nonparametric test or Fisher exact test for continuous variables or categorical variables. Two-sided p -value of < 0.05 was considered statistically significant. To compare the percentage of screw malposition between the two treatment groups, the univariate weighted generalized linear model was conducted assuming the percentage and number of malpositions to be gamma distributed. The total number of LMS was used as weighted values, and the GENMOD procedure was applied for this analysis in the SAS (SAS version 9.4 for Windows). The outcome of the model was the percentage of screw malposition.

Results

The median age of the patients was 64 years, and 60% of the total patients were males. The median hospital stay was found to be 5 days, and nobody had SCI, VAI, or NRI. The median number of LMS was 8, and none of the patients had any screw breakage, pull out, or loosening (► **Table 1**).

The two groups of patients have been compared in ► **Table 2** for better evaluation of the patients' demographics and clinical outcomes.

As shown in ► **Table 2**, there is no statistically significant difference between the two groups in terms of demographic data (age, gender), number of LMS per patient, number of trauma patients, and extension of instrumentation. There was also no significant difference between the two groups in terms of LMF, blood loss, and hospital stay, but the two groups showed a significant difference in the operation time ($p = 0.045$). That is because the time required for the application and registration of the 3D navigation. Also, we compared each level of instrumentation and showed no significant difference between the two groups (► **Table 3**).

In the 3D navigation system group, 144 screws were used in total, and 16 screws were malpositioned. On the other hand, in the freehand technique group, the total number of screws was 140, and the number of malpositioned screws was 27.

Among 284 total number of LMS, there were 19.3% screw malpositions in the freehand technique (140 LMS), and 11.1% malpositions in the 3D neuronavigation technique (144 LMS). To compare percentage of malpositions between two treatment groups, weighted generalized linear model was conducted (► **Table 4**). There was a significant difference between the percentage of screw malposition between the

Table 1 Shows the basic information of all the 40 patients

Demographics		
Age (y)		
N	40	
Mean ± SD	63.3 ± 10.9	
Median (interquartiles)	64 (55, 71)	
Range	44, 93	
Gender		
Female	16	(40.00%)
Male	24	(60.00%)
Clinical outcomes		
Treatment group		
Freehand technique	20	(50.00%)
3D navigation system	20	(50.00%)
Screw/Rod breakage		
No	40	(100.00%)
Yes	0	(0.00%)
Screw pullout		
No	40	(100.00%)
Yes	0	(0.00%)
Screw loosening		
No	40	(100.00%)
Yes	0	(0.00%)
Hospital stays (d)		
N	40	
Mean ± SD	7.3 ± 5.5	
Median (interquartiles)	5 (3, 11)	
Range	2, 24	
Vertebral artery injury		
No	40	(100.00%)
Yes	0	(0.00%)
Spinal cord injury		
No	40	(100.00%)
Yes	0	(0.00%)
Nerve root injury		
No	40	(100.00%)
Yes	0	(0.00%)
Instrumentation		
Thoracic		
No	30	(75.00%)
Yes	10	(25.00%)
Occipitocervical		
No	36	(90.00%)
Yes	4	(10.00%)

Abbreviation: SD, standard deviation.

3D navigation and freehand technique ($p = 0.0103$) (\rightarrow **Table 5**). Patients using the freehand technique are more likely to have higher percentage of screw malpositions compared with those using the 3D navigation system (due

Table 2 Demographics and clinical outcomes

	3D navigation group (n = 20)	Freehand group (n = 20)	p-Value ^a
Age (y)			
Mean ± SD	62.0 ± 13.1	64.6 ± 8.4	0.2847
Range	44–93	44–81	
Gender			
Female	9 (45%)	7 (35%)	0.7475
Male	11 (55%)	13 (65%)	
No. of LMS/patient median	8	8	0.9772
Pathology of trauma	8 (40%)	6 (30%)	0.7411
Cervicothoracic extension	6 (30%)	4 (20%)	0.716
Occipitocervical extension	1 (5%)	3 (15%)	0.605
Operative time (h) (mean ± SD)	5.1 ± 1.32	4.35 ± 1.67	0.0453
Blood loss (mean ± SD)	615 ± 629.8	574.7 ± 350.9	0.3766
IOM	7 (35%)	6 (30%)	0.7357
LMF	1 (5%)	4 (20%)	0.3416
Neurological deficit	3 (15%)	1(5%)	0.6050
Reoperation	0 (0%)	2 (10%)	0.4872
Hospital stay (d) (mean ± SD)	8.1 ± 5.9	6.5 ± 5.0	0.4536

Abbreviations: IOM, intraoperative monitoring; LMF, lateral mass fracture; LMS, lateral mass screw; SD, standard deviation.

^ap-Value of < 0.05 was considered statistically significant.

Table 3 Each level instrumentation

Level	Freehand group	3D navigation group
C3	30	30
C4	33	39
C5	34	39
C6	31	32
C7	12	4
Total	140	144

to negative coefficient). The goodness-of-fit shows how well our assumption of gamma distribution fits the real data. The scaled deviation and scaled Pearson's chi-squared test were both close to one, indicating that the underlying distribution was indeed close to the gamma distribution.

There was also a significant difference in the number of screw malpositions between both the techniques ($p = 0.0323$). The patients using the freehand technique are more likely to have a higher number of screw malpositions compared with

Table 4 Shows the weighted mean percentage of screw malpositions

	Total (no. of screws = 284)	Freehand technique (no. of screws = 140)	3D navigation system (no. of screws = 144)
No. of subjects	40	20	20
No. of screws	284	140	144
% of screw malpositions			
Weighted mean \pm SD	15.14 \pm 41.00	19.29 \pm 49.59	11.11 \pm 27.22
Median (interquartiles)	12.5 (0, 25)	14.6 (0, 25)	12.5 (0, 17)
Range	0, 57	0, 57	0, 33
Screw malpositions			
Weighted mean \pm SD	1.10 \pm 2.96	1.36 \pm 3.56	0.85 \pm 2.09
Median (interquartiles)	1.0 (0, 2)	1.0 (0, 2)	1.0 (0, 1)
Range	0, 4	0, 4	0, 2

Abbreviation: SD, standard deviation.

Table 5 Comparing the percentage of screw malpositions

Comparing the percentage of screw malpositions	Coefficient	SE	p-Value
Intercept	3.3367	0.1244	< 0.0001
Group (3D navigation versus freehand)	-0.4587	0.1788	0.0103

Abbreviation: SE, standard error.

Note: Goodness of fit: Scaled deviance = 1.1228; Scaled Pearson χ^2 = 1.1139.

Table 6 Comparing no. of screw malposition

Comparing no. of screw malposition	Coefficient	SE	p-Value
Intercept	0.6879	0.1247	< 0.0001
Group (3D navigation versus freehand)	-0.3837	0.1791	0.0323

Abbreviation: SE, standard error.

Note: Goodness of fit: Scaled deviance = 1.1230; Scaled Pearson χ^2 = 1.1672.

those using the 3D navigation system (due to negative coefficient) (**Table 6**).

► **Table 7** shows coefficient, standard error (SE) of coefficient, and *p*-value of each clinical predictive factor; the goodness-of-fit shows how well our assumption of gamma distribution fits the real data. If the scaled deviation and scaled Pearson's chi-square are both closer to one, it indicates that the underlying distribution is indeed close to a gamma distribution. In the univariate weighted generalized linear regression analysis, gender has a borderline *p*-value of 0.0593.

In the multivariate analysis, all significant variables obtained from the univariate generalized linear model were put into one big model. We also put gender into the multiple regression model due to its borderline *p*-value. In the below model (**Table 8**), only LMF remained significant (*p* = 0.0294) after adjusting for other factors. The patients with LMF have

a significantly higher percentage of screw malpositions compared with others. The weighted mean of screw malposition percentage was 39.4% in patients with LMF and 12.0% in patients without LMF.

Discussion

The use of LMS in cervical spine instrumentation has been proven to be effective in stabilizing the cervical spine with various kinds of pathology.^{7,12,15–18} The usage of the polyaxial screw with rods is the principal device of choice for posterior stabilization of the cervical spine, especially when the upward or downward extension is required.^{7,19}

Both cervical pedicle screws and LMS have their advantages and disadvantages. Cervical pedicle screw instrumentation offers rigid fixation but with risk to VAI.^{7,20,21} Unlike cervical pedicle screws, LMS placement requires a shorter learning period and is a more straightforward surgical procedure.⁷ The principal complications caused by LMS malposition are a violation of vertebral arteries and cervical NRI.²²

We used the Ching technique, a simple and uniform method for placing LMS from C3 to C7, by proposing a modification technique that shifted the screw entry point to 1.5 mm medial and inferior to the geometrical center of the LMS.⁷ In 1995, Pait et al²³ divided the lateral cervical mass (articular pillars of the cervical spine) into quadrants and concluded that the superior lateral quadrant was the “safe quadrant” for placing LMS. The Ching technique entry point combined with the trajectory allows also to aim at the “safe quadrant.”^{24,25} One of the main reasons we can follow such a greatly angulated trajectory is the development of polyaxial screws.⁷ We used the modified Magerl technique (Ching) because it is safe for the VA and the spinal nerve. Overall, the nerve and artery were safe from compromise at levels C3 to C6 with lateral angulation of 20°, 25° (standard), and 30°.²⁶

Generally, the application of 3D neuronavigation techniques in the cervical spine appears to increase the accuracy,¹ with the misplacement rates ranging from 2 to 40%.^{9,27,28} Holly et al reported that the paired point matching

Table 7 The coefficient, SE of coefficient, and *p*-value of each clinical predictive factor

Predictive factor	Coefficient	SE	<i>p</i> -Value ^a	Scaled deviance	Scaled Pearson χ^2
IOM (Yes versus No)	0.3418	0.2027	0.0917	1.127	1.313
Operation time (continuous)	0.1091	0.1226	0.3736	1.131	1.304
Operation time ≥ 4.3 versus < 4.3	0.2789	0.1938	0.1502	1.129	1.338
Blood loss (continuous)	0.1384	0.1278	0.2790	1.130	1.381
Blood loss ≥ 450 versus < 450	0.1646	0.2012	0.4132	1.131	1.325
Neurological status (deficit versus Intact)	0.2271	0.3511	0.5179	1.131	1.295
Age (y)	0.0047	0.0106	0.6596	1.132	1.353
Age (≥ 65 y versus < 65 y)	0.0690	0.1995	0.7295	1.132	1.349
Gender (Male versus Female)	0.3747	0.1987	0.0593	1.127	1.160
Hospital stay (≥ 5 d versus < 5 d)	-0.1777	0.1960	0.3647	1.130	1.316

Abbreviation: IOM, intraoperative monitoring; SE, standard error.

^a*p*-Value < 0.05 was considered statistically significant.

Table 8 After adjusting of other factors

Predictive factor	Coefficient	SE	<i>p</i> -Value ^a	Scaled deviance	Scaled Pearson χ^2
Intercept	2.8615	0.1425	< 0.0001	1.270	1.266
Lateral mass fracture (Yes versus No)	0.4869	0.2235	0.0294		
Gender (Male versus Female)	0.2597	0.1619	0.1086		
Reoperation (Yes versus No)	0.4374	0.4397	0.3198		
Thoracic (Yes versus No)	-0.2676	0.1924	0.1642		

Abbreviation: SE, standard error.

^a*p*-Value < 0.05 was considered statistically significant.

supplemented with surface matching resulted in a lower mean registration error than the paired point matching alone.¹⁹ The intertechnique difference in navigational error was nearly equivalent (1.3 mm compared with 1.4 mm) and statistically insignificant.¹⁹

LMS fixation is a relatively safe procedure; however, there are several complications that may be encountered during LMS insertion, such as VAI, NRIs, facet violation, and LMF,^{1,16} due to LMS malposition. In the analysis of clinical results, Graham et al and Roche et al claimed that the screw positioning is the main factor leading to the complications related to LMS.^{1,29,30} "In cadaveric experiments simulating the surgical procedure, Heller et al,¹⁴ Seybold et al,¹³ and Barrey et al³¹ showed a correlation between the risk of these complications and an inappropriate screw trajectory angle."¹ In our study, there were 19.3% of screw malpositions in the freehand technique (140 LMS) and 11.1% of malpositions in the 3D navigation system (144 LMS). There was a significant difference in the percentage of screw malpositions between the 3D navigation and freehand techniques ($p = 0.0103$). In our study, there were no VAIs, SCI, or NRI.

Several reports have demonstrated the malposition of LMS to be a potential risk factor for facet violation (FV) and FT that may lead to complications. Ebraheim et al³² reported that the violation of the inferior facet of the most caudal facet joint may lead to revision surgery to extend the fixation.¹ Moreover, Shinichi stated that the violation of FT or FV is related to the

malposition of LMS trajectory in the axial or sagittal planes, respectively.¹ The anatomic study of An et al⁴ observed that the nerve roots' exit point was at the anterolateral portion of the superior facet and that the malposition of LMS with the violation of the superior facet may lead to NRI.

A few clinical papers referred to the LMF with an incidence of 1.6 to 4%.^{1,18,33-35} Our study showed 15% LMF in the freehand technique compared with 5% in the 3D neuronavigation technique with an insignificant *p*-value (0.3416). From the statistical analysis, the patients with LMF have a significantly higher percentage of screw malpositions compared with others. We followed the same management of Inoue et al to deal with intraoperative LMF by abandoning screw insertion at the corresponding level of all lateral masses with fractures.³³ Katonis et al reported that the lateral screw trajectory (malposition) increased the incidence of LMF.^{33,34}

The limitation of this study is that the surgeries were performed by multiple surgeons, and this could affect the accuracy of the entry point and screw trajectories. However, the strength factor of our study is that we had a postoperative CT scan for each patient. We also involved an independent interobserver to analyze the screws. In addition to the LMS fixation, we used the modified Magerl technique, which reduced the complication rate for the freehand group because of its safe trajectories. The use of the 3D navigation for the second group with preop loading of CT scans also gave us better trajectories and starting points.

Conclusion

The use of 3D navigation decreased the malpositions in LMS instrumentation compared with the freehand technique (modified Magerl). Also, the patients with LMF have a significantly higher percentage of screw malpositions compared with others. The study did not show any significant difference in VAI, NRI, SCI, screws complications, or blood loss between the two groups. We recommend that future studies should further investigate the effect of malpositions on the biomechanics of the cervical spine and its clinical application.

Conflict of Interest

None.

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