Dual-Energy Perfusion-CT in Recurrent Pancreatic Cancer – Preliminary Results

Dual-Energy Perfusion-CT bei Pankreaskarzinomrezidiven – Vorläufige Ergebnisse

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Abstract
Purpose: To evaluate the diagnostic performance of dual energy (DE) perfusion-CT for the differentiation between postoperative soft-tissue formation and tumor recurrence in patients after potentially curative pancreatic cancer resection.

Material and Methods: 24 patients with potentially curative pancreatic cancer resection with curative intent were included prospectively. They were examined with a 64-row dual-source CT using a dynamic sequence of 34 DE acquisitions every 1.5 s (80 ml of iodinated contrast material, 370 mg/ml, flow rate 5 ml/s). Weighted average (linearly blended M0.5) 120 kVp-equivalent dual-energy perfusion image data sets were evaluated with a body-perfusion CT tool (see above) for estimating blood flow, permeability, and blood volume. Diagnosis was confirmed by histological study (n = 4) and by regular follow-up.

Results: Final diagnosis was local recurrence of pancreatic cancer in 15 patients and unspecific postoperative tissue formation in 9 patients. The blood-flow values for recurrence tissue trended to be lower compared to postoperative tissue formation with 16.6 ml/100 ml/min and 24.7 ml/100 ml/min, respectively for weighted average 120 kVp-equivalent image data, which was not significant (n.s.) (p = 0.06, significance level 0.05). Permeability- and blood-volume values were only slightly lower in recurrence tissue (n.s.).

Conclusion: DE perfusion-CT is feasible in patients after pancreatic cancer resection and a promising functional imaging technique. As only a trend for lower perfusion values in local recurrence compared to unspecific postoperative alterations was found, the perfusion differences are not yet sufficient to differentiate between malignancy and unspecific postoperative alterations for this new technique. Further studies and technical improve-
schen, postoperativen Weichgewebeformationen nachzuweisen; die Perfusionsunterschiede reichen aktuell noch nicht aus, um zwi-
schen malignen und unspezifischen, postoperativen Veränderun-
gen zu differenzieren. Weitere Studien sowie technische Verbesser-
ungen sind nötig, um verlässliche Werte für die Beantwortung
der problematisch hochrelevante Frage zu erhalten.

Kernaussagen:

► DE Perfusion-CT ist ein machbares, technisch hochrelevantes Mittel, das zur differenzierung von Rezidiven in der rein morphologischen Diagnostik von Pankreaskarzinom-Rezidiven zu überwinden.

Introduction

Pancreatic cancer is known to have poor prognosis since the ma-

jority of patients present with advanced tumor stages at the time

doagnosis, which allows a potentially curative resection in only

approximately 20% of the patients [1]. Following potentially cure-

tive surgery, isolated local recurrence occurs in one third of

the patients [1, 2].

In cases of local recurrence without distant metastases, however,

patients may benefit from surgery, which was shown to be asso-
ciated with an additional 15 months median overall survival [3].

Therefore, it is essential to identify local tumor recurrence early

as this offers the possibility of recurrence resection, which can be

combined with radiotherapy to achieve best results [4, 5]. To

achieve this goal, a close follow-up following pancreatic ductal

adenocarcinoma (PDAC) resection is required [4, 6, 7]. The Na-
thional Comprehensive Cancer Network (NCCN) guidelines recom-

mend a close surveillance with clinical history, physical examina-
tion, CA 19-9 and CT every 3 to 6 months for the first two years

and then annually [8].

The major problem in detecting pancreatic cancer recurrence by

CT-based follow-up is caused by unspecific postoperative chang-
es with soft-tissue formation that can often barely be differenti-
ated from disease recurrence [9]. Local recurrence is suspected in

contrast-enhanced (CE-) CT if there is a visible enlargement of

preexisting soft-tissue formations or if new soft-tissue forma-
tions appear.

Conventional CECT offers high-resolution imaging and is widely

available, safe and fast, but is only a morphology-based imaging

method. Using perfusion CT offers the opportunity to get addi-
tional functional imaging information of the examined parench-
yma with the same high resolution as provided by conventional

CT. This implies that quantitative parameters like blood flow of

the examined tissue can be quantified. Additionally, perfusion

CT can be performed in dual energy mode, which offers image

data featuring the enhanced contrast at 80 kVp while having the

noise characteristics of an acquisition at 140 kVp. Many studies

have shown the feasibility and value of perfusion CT and DE per-

fusion-CT in pancreatic cancer [10–12], but to our knowledge

there are so far no publications on the topic of perfusion CT in

pancreatic cancer recurrence.

The purpose of our study was to evaluate the possibility of differ-

entiating unspecific postoperative soft-tissue alterations from tu-
mor recurrence in the follow-up of patients after pancreatic can-
cer resection using DE perfusion-CT.

Material and Methods

Patient collective

This prospective study was approved by the Institutional Review

Board. Every enrolled patient provided written informed consent

with notice about the additional radiation exposure of the perfu-
sion sequences. Inclusion criteria were patients with pancreatic

adenocarcinoma preceding resection, who were scheduled for

regular follow-up CT at our institution (in-house protocol initi-
ates follow-up three month after resection) and on who conven-
tional CT detected soft-tissue formation in the anatomical area of

the preceding operation suggestive of recurrence. Exclusion

criteria for perfusion CT were: general contraindications for the

application of contrast medium, previous treatment for recur-

cence of pancreatic carcinoma, inability to reproduce the breath-
ing technique (see below).

The final diagnosis of pancreatic cancer recurrence was made his-
topathologically after surgery. If no repeat resection was per-
formed the progression of CT- and clinical findings during fol-

low-up served as standard of reference for diagnosing local

recurrence.

After primary diagnosis n = 11 patients in the group of recurren-
ces that had Whipple’s procedures, n = 2 had left side pancreatic re-
section and n = 2 had total pancreatectomy. In the group of post-
operative soft-tissue formations there were n = 6 Whipple’s proc-
cedures, n = 1 left side pancreatic resection and n = 2 had total

pancreatectomy.

In the group of patients with recurrences R0 resection was

achieved in n = 7 patients, there were n = 14 T3-stages and n = 1

T1-stage, n = 14 had positive lymph node stages. In the group of

postoperative soft-tissue formations R0 resection was achieved in

n = 1 patient, there were n = 9 T3-stages and n = 6 positive

lymph node stages.

One patient with postoperative soft-tissue formation was enrol-
led twice in this study, but only the first examination was in-
cluded in the analysis.

CT imaging

Prior to the CT acquisition, patients had to drink 1 – 1.5 liters of

water and received 20 mg of hyoscine butylbromide i. v. (Busco-
pan®, Boehringer, Ingelheim, Germany) [13].

The patients were examined with a 64-row dual-source CT (Sie-
mens Somatom Definition Flash, Erlangen, Germany). First we per-
formed a helical CT-acquisition of the abdomen before and after

administration of 80 ml of non-ionic iodinated contrast material

ments are needed to generate reliable data for this clinically highly

relevant differentiation.

Key points:

► DE Perfusion CT is feasible in patients after pancreatic cancer

resection.

► While reliable differentiation of unspecific postoperative tis-

sue formation from recurrent malignancy cannot be achieved

yet, it is within reach.

► DE Perfusion CT has the potential to overcome today’s limita-

tions of pure morphological diagnosis of recurrent pancreatic

cancer.

Citation Format:

► Fritz F, Skornitzke S, Hackert T et al. Dual-Energy Perfusion-CT

in Recurrent Pancreatic Cancer – Preliminary Results. Fortschr

Röntgenstr 2016; 188: 559–565

Fritz F et al. Dual-Energy Perfusion-CT in... Fortschr Röntgenstr 2016; 188: 559–565
(370 mg iodine/ml; Ultravist® 370, Schering, Berlin, Germany), including at least arterial and venous phases (table 1). After conventional CT-acquisition of the upper abdomen, there was a 15 minute break to allow for contrast material to wash-out from the pancreatic parenchyma. During this break the patients remained on the CT table without moving. In order to minimize breathing artefacts during the following dynamic CT-examination, patients were instructed to use a shallow breathing technique. During the waiting period we defined the localization of the suspicious soft-tissue formation based on the CECT acquisition. A single low-dose acquisition (scan-&-view) during shallow breathing was used to validate the correctness of the chosen acquisition region. For the perfusion sequence 80 ml of a non-ionic contrast material (370 mg iodine/ml; Ultravist® 370, Schering, Berlin, Germany) was injected through a 16- or 18-gauge catheter in an antecubital vein using a flow rate of 5 ml/s, followed by a chaser bolus of 40 ml saline solution. The perfusion sequence in dual-energy mode was started after a constant delay of 13 seconds with respect to contrast material injection. The dual-energy (DE) technique employed tube voltages of 80 kVp and 140 kVp using tin filtration with effective tube currents of 270 mAs and 104 mAs (CARE Dose 4D, Siemens Medical Solutions, Forchheim, Germany) respectively. The dynamic imaging sequence consisted of 34 acquisitions of 0.5 s duration (rotation time) every 1.5 s (cycle time) (total examination time of 51 s). The perfusion sequence covered a craniocaudal width of 19.2 mm (collimation of 32 × 0.6, table 1) from which three consecutive image slices of 5 mm slice thickness could be reconstructed for each of the 34 acquisitions (kernel B30 f (n = 16), B31 f (n = 8)).

Data analysis
Perfusion data were analyzed utilizing a Body-Perfusion CT-tool (CT Body Perfusion – Workflow Template, Siemens Medical Solutions, Erlangen, Germany) at a multimodality workplace with the syngo.via imaging software (Siemens Medical Solutions, Forchheim, Germany). The CT Body Perfusion application (pancreatic tumors) for appraisal of perfusion data is based inter alia on compartment models. For the estimation of the blood flow value a single-compartment-model (maximum slope) and for blood volume value and flow extraction value a two-compartment model (Patlak) is used [14, 15]. We evaluated the weighted average (linearly blended M0.5) 120 kVp-equivalent examinations of the dual-energy acquisition with a B30 f kernel (n = 16) or a B31 f kernel (n = 8) to estimate the parameters and parameter maps.

Table 1: Protocol of the three-phasic CT-acquisition and the dynamic DECT-perfusion sequence.

<table>
<thead>
<tr>
<th>phase</th>
<th>tube potential [kVp]</th>
<th>tube current (eff.) [mAs]</th>
<th>primary collimation [mm]</th>
<th>slice thickness (recon.) [mm]</th>
<th>delay [s]</th>
<th>gantry rotation time [s]</th>
<th>number of acquisitions</th>
</tr>
</thead>
<tbody>
<tr>
<td>1. native</td>
<td>120</td>
<td>210&lt;sup&gt;1&lt;/sup&gt;</td>
<td>2 × 64 × 0.6</td>
<td>3.0/1.5</td>
<td>4</td>
<td>0.5</td>
<td>helical</td>
</tr>
<tr>
<td>contrast medium: 80 ml (flow 5 ml/s); ROI: abdominal aorta at the level of the coeliac trunk; trigger threshold: 120 HU; cycle time: 1.5 s; monitor delay: 10 s</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>2. arterial</td>
<td>120</td>
<td>210&lt;sup&gt;1&lt;/sup&gt;</td>
<td>2 × 64 × 0.6</td>
<td>3.0/1.5</td>
<td>10</td>
<td>0.5</td>
<td>helical</td>
</tr>
<tr>
<td>3. venous</td>
<td>120</td>
<td>210&lt;sup&gt;1&lt;/sup&gt;</td>
<td>2 × 64 × 0.6</td>
<td>3.0/1.5</td>
<td>40</td>
<td>0.5</td>
<td>helical</td>
</tr>
<tr>
<td>15 minutes break: contrast medium clearance – patient remaining on the CT table</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>contrast medium: 80 ml with 40 ml saline solution chaser (flow 5 ml/s)</td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
<td></td>
</tr>
<tr>
<td>4. perfusion</td>
<td>3n140/80</td>
<td>104/270</td>
<td>32 × 0.6</td>
<td>3 × 5.0</td>
<td>13</td>
<td>0.5 (full rotation)</td>
<td>34 dynamic</td>
</tr>
</tbody>
</table>

KVP = peak kilovoltage; mAs = milliampere-second; eff. = effective; mm = millimeter; ml = milliliter; recon. = reconstructed; s = second; HU = Hounsfield Units; Sn = tin filtration, Siemens; 1 plus CARE Dose 4 D and CARE kV, Siemens.

Two radiologists (with twelve years and four years of experience in interpreting abdominal images, respectively) placed polygonal VOIs in the suspicious tissue formation. Therefore, a joint decision for placing the VOI was made, trying to cover as much suspicious tissue as possible without including any vessels. Using a compartment model the software calculated the following parameters, respectively:

- perfusion [ml/100 ml/min]
- permeability [ml/100 ml/min and]
- blood volume [ml/100ml]

Radiation exposure
Effective radiation dose (D<sub>eff</sub>) was calculated for the DE-acquisition of the perfusion sequence including the contribution of both tubes operating at 80 kVp and 140 kVp, respectively, as well as for the acquisitions in the context of regular follow-up CT examination. For that purpose, each of the corresponding dose-length-products (DLP) were multiplied with the corresponding conversion factor for abdominal CT-examinations (0.015 mSv/mGy · cm based on ICRP 60 published in 2004) [16]. Thus, the total radiation exposure (RE) of the CT examination is the sum of the effective radiation doses D<sub>eff</sub> of the dynamic DE-perfusion sequence as well as of the single-energy acquisitions.

Statistical analysis
For quantitative analysis, the distribution of the patient age and CT-perfusion-parameters was given as mean value with standard deviation and range. The derived perfusion-parameters were tested for significant differences between pancreatic cancer recurrence and unspecific soft tissue using an unpaired t-test, respectively. A significance level of p < 0.05 was considered statistically significant. Descriptive statistics as well as t-tests were performed using Microsoft® Excel® 2008 for Mac, Version 12.3.6. Box-plots were generated using R (R Foundation for Statistical Computing).
Results

The study population consisted of 24 patients (16 men, 8 women) (mean age 66.2 years; range: 48 – 83). The mean follow-up period in the group of postoperative soft tissue formation was 42.4 months. During this period no suspicious growth was detected in the regular follow-up CT. In the group with pancreatic cancer recurrence mean follow-up was 14.7 months.

DECT perfusion was feasible and could be evaluated in all 24 patients. The final diagnosis was local recurrence of pancreatic cancer in 15 patients. In nine patients postoperative soft-tissue formation without local recurrence was diagnosed. Out of the 15 patients with recurrence histological proof of local recurrence was available in four patients, while the remaining 11 patients showed typical symptoms of progressive disease in the further follow-up confirming the diagnosis. The mean diameter of the recurrent tissue formations was 1.9 × 2.5 cm, while the diameter of the non-tumorous postoperative tissue averaged 1.2 × 2.1 cm.

In Fig. 1 the box-plot exemplifies the data points of the blood flow in recurrence versus postoperative soft-tissue formations. The mean values with standard deviation for blood flow, permeability and blood volume in recurrence and unspecific postoperative tissue formations for weighted average 120kVp-equivalent DE image data are visualized in Fig. 2, 3 and summarized in Table 2.

The blood-flow values for recurrence tissue were lower compared to postoperative soft tissue with a range from [8.4 – 29.9] ml/100 ml/min for weighted average 120 kVp-equivalent image data in recurrence and a range from [9.9 – 66.9] ml/100 ml/min for weighted average 120kVp-equivalent image data in postoperative soft-tissue formation. These differences did not reach statistical significance (p = 0.06).

Mean permeability values were lower in recurrence tissue compared to postoperative soft tissue with a range from [0.9 – 17.1] ml/100 ml/min and [1.6 – 29.7] ml/100 ml/min for weighted average 120 kVp-equivalent image data (n.s.).

The blood volume values were nearly the same in recurrence and postoperative soft tissue (range: 0.1 – 6.2 ml/100 ml and 0.04 – 5.96 ml/100 ml) for weighted average 120 kVp-equivalent image data (n.s.; Table 2).

Radiation exposure

The mean total radiation exposure (DLP) for the entire CT examination (regular follow-up CT plus dynamic perfusion sequence) was 1248.9 mGy × cm (Deff (total) = 18.7 mSv) subdivided in 598.8 mGy × cm (Deff (DECT perfusion) = 9.0 mSv) for the perfusion sequence [range 258 – 761 mGy × cm (Deff = 3.9 – 11.4 mSv)] and 650.1 mGy × cm (Deff (3-phase CT) = 9.7 mSv) for the regular follow-up CT [range 260 – 1362 mGy × cm (Deff = 3.9 – 20.4 mSv)].

In line with the regular follow-up acquisitions all patients had
Local recurrence of pancreatic cancer occurs in 80% of patients undergoing potentially curative resection [17]. Patients with isolated local recurrence of pancreatic cancer showed the potential of dual-energy perfusion-CT in patients with pancreatic carcinoma by more accurate measurements compared to single-energy perfusion-CT [11].

One previous dual-energy perfusion-CT study in pancreatic cancer showed the potential of dual-energy perfusion-CT in patients with pancreatic carcinoma by more accurate measurements compared to single-energy perfusion-CT [11].

Our findings of non-significantly reduced blood-flow values in pancreatic cancer recurrence tissue compared to non-tumorous postoperative soft tissue tend to match the results of CT perfusion studies evaluating primary pancreatic cancer. These studies reported reduced blood flow in pancreatic adenocarcinomas.

Table 2  Mean values with standard deviation of blood flow, permeability and blood volume for recurrence and postoperative soft-tissue formation after pancreatic cancer resection at average weighted 120kVp examinations.

<table>
<thead>
<tr>
<th>Parameter</th>
<th>Recurrence tissue (n = 15)</th>
<th>Postoperative soft tissue (n = 9)</th>
<th>p-value</th>
</tr>
</thead>
<tbody>
<tr>
<td>Blood flow [ml/100 ml/min]</td>
<td>16.6 ± 6.0</td>
<td>24.7 ± 18.1</td>
<td>0.06</td>
</tr>
<tr>
<td>Permeability [ml/100 ml/min]</td>
<td>8.7 ± 4.0</td>
<td>10.7 ± 9.3</td>
<td>0.23</td>
</tr>
<tr>
<td>Blood volume [ml/100ml]</td>
<td>2.3 ± 1.6</td>
<td>2.8 ± 1.8</td>
<td>0.25</td>
</tr>
</tbody>
</table>

ml = milliliter; min = minute.

terstitial and venous phases, n = 11 also had non-enhanced phases, n = 9 had additional venous chest CT and n = 5 patients had late venous phases due to inexplicit lesions.

**Discussion**

In the present study, dual source dual energy CT perfusion has been used for the first time to differentiate local disease recurrence from unspecific soft-tissue alterations in patients after pancreatic cancer resection. We found that while local disease recurrence shows lower blood flow than postoperative soft-tissue formation, there was a considerable overlap between both groups.

Local recurrence of pancreatic cancer occurs in 80% of patients within 2 years after potentially curative resection [17]. Patients with isolated local recurrence of pancreatic cancer show a survival benefit when repeat resection [3] with or without radiotherapy can be performed [18], and should therefore be identified early during follow-up. One of the most difficult radiological challenges in this context is the differentiation between unspecific postoperative soft-tissue alterations and true recurrence at an early stage with conventional imaging modalities.

In some cancer centers, postoperative follow-up with PET-CT imaging after pancreatic cancer resection is performed under the assumption that this imaging method is superior in identifying pancreatic cancer relapse compared to CECT [19, 20]. This is, however, a costly and not widely available method. Consequently, a postoperative follow-up protocol including regular CECT and tumor marker measurement as a cost-effective standard is used in most centers, and PET-CT is performed only in cases of inconclusive CT and tumor marker/clinical findings [4]. A new complementary CT technique providing additional functional information on the examined tissue, such as CT perfusion and dual-energy CT could overcome the disadvantage of CECT compared to PET-CT, with the benefit of greater availability and lower costs. Dual-energy CT and perfusion-CT as well as the combination thereof are expected to improve the diagnosis of pancreatic cancer [11, 21 – 23]. Using perfusion-CT, the analysis of temporal changes of attenuation (in Hounsfield units [HU]) allows assessing the vascular supply of tumors. The derived blood flow values correlate with the histopathologically determined microvessel density in pancreatic neuroendocrine tumors [24]. Dual-energy CT offers the possibility of a simultaneous data acquisition using different photon spectra (usually at 80/100 kVp and 140 kVp) of distinctly different mean energies during a single helical acquisition [25]. The thereby derived weighted average 120 kVp-equivalent image data combine the advantages of increased (iodine) contrast at 80 kVp with the low noise at 140 kVp, and could thus improve the delineation of perfusion differences between pancreatic cancer recurrence and postoperative soft-tissue alterations.

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compared to healthy pancreatic tissue both in dual-energy perfusion-CT as well as single-energy perfusion-CT [12]. Our findings suggest that local pancreatic cancer regrowth induces changes leading to a reduced tissue-perfusion, similar to primary pancreatic cancer growing in healthy pancreatic tissue. Histopathologically confirmed pancreatic cancer recurrences show similar changes as primary pancreatic tumors with desmoplastically altered tissue with fibrous stroma and epithelioid tumor cells [26], which explain a reduced blood flow in these lesions. Compared to the reported blood-flow values of pancreatic cancer in previous dual-energy and single-energy studies, the blood-flow values of local recurrence of pancreatic cancer in our study were even lower, with mean values of 17 ± 6 *0.01 min⁻¹ vs. 27 ± 4 "0.01 min⁻¹ and 32 ± 28 "0.01 min⁻¹ [10, 11]. This can be explained by the perfusion characteristic of the underlying environmental tissue in which the respective lesions develop.

As both postoperative soft tissue and pancreatic recurrence tissue have very low blood volume values we could not find significant differences between the two. The permeability values in pancreatic cancer recurrence compared to non-tumorous postoperative soft tissue were in the same range with a slight trend towards lower permeability values in cancer regrowth. This finding again matches the results of the comparison between pancreatic cancer and healthy pancreatic tissue. The values tended to be lower in pancreatic cancer, but without significant difference and a wide range in values [11, 12]. In earlier perfusion-CT studies, permeability values for local recurrence of pancreatic cancer compared to primary pancreatic cancer were clearly lower which is in line with the finding of the present study. We found a mean permeability of approximately one-fourth of the reported permeability-values in pancreatic cancer tissue [11, 12].

A limitation of the study is the small number of patients without local recurrence of pancreatic cancer. Further studies including more patients are needed to confirm the trend we found between recurrence and non-tumorous postoperative soft tissue. Secondly we did not obtain histological confirmation of the suspected recurrence in all patients. The local recurrences that were diagnosed by further signs of progression in the following examinations already showed a measurable progression in size compared to former CT at the time of examination with the perfusion-CT-protocol. Nevertheless, it is possible that the soft-tissue formation at the time of examination with the perfusion-protocol was not representative for recurrent malignant tissue in the perfusion-CT. Therefore an overestimation of local recurrence in this study is possible. Further studies with regular integration of dual-energy-/perfusion-imaging could solve this problem by recording functional parameters during the course of follow-up, but significant dose-reduction would thus be required.

Furthermore, there was no histological confirmation in patients with unspecified postoperative soft-tissue formation due to the corresponding small alterations, which are not easily accessible for puncture, for example. However, we supposed a comparatively long period of follow-up without any signs of progression in these patients long enough to assume that these changes do not have primary malignant behaviour.

In conclusion, dual-energy perfusion CT is feasible in patients after pancreatic cancer resection and is a promising functional imaging technique. As we only found a trend to lower perfusion values in local recurrence compared to unspecified postoperative tissue alterations, the perfusion differences between both tissues are not yet sufficient to allow a clear distinction. Further studies including larger patient collectives and technical improvements are needed to achieve reliable data for this differentiation.

Acknowledgements

This research was supported by the German Research Foundation (DFG) within project R02 entitled “Innovative Imaging of Tissue Perfusion” of the Transregional Collaborative Research Center SFB/TRR 125 “Cognition-guided Surgery”.

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