

# Evaluation of the New DIN Standard for Quality Assurance of Diagnostic Displays – Technical Review DIN 6868-157

## Evaluation der neuen DIN-Norm für Qualitätssicherungen an Monitoren in der Radiologie – Technical Review DIN 6868-157

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### ABSTRACT

Acceptance and regular constancy tests are necessary to ensure the quality of diagnostic displays. In November 2014, a new standard (DIN 6868-157) was published which defines the test procedure and limiting values. There are several substantial changes compared with the previous standard DIN V 6868-57, i. e. considering the complete image display system including workstation and application software instead of only the displays. Since its publication, the new standard has raised many questions. This technical review aims to show the strengths and weaknesses of the new standard. Positive aspects are the introduction of a limiting value for the illuminance and the extension of the interval for con-

stancy tests from 3 to 6 six months. The daily constancy test on the other hand, raises several problems and should be replaced by a randomized test. Additionally, the medical relevance is critically questioned and an overview of software for the quality assurance will be given.

### Key points

- Acceptance and constancy tests for diagnostic displays are defined in DIN 6868-157.
- The new standards has positive and negative aspects.
- Randomized tests should be introduced.

### Citation Format

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### ZUSAMMENFASSUNG

Zur Sicherung der Bildqualität müssen an Befundmonitoren Abnahme- und regelmäßige Konstanzprüfungen durchgeführt werden. Im November 2014 ist eine neue DIN-Norm erschienen (DIN 6868-157), die den Prüfablauf regelt und Grenzwerte festlegt. Im Vergleich zur bisherigen DIN-Norm DIN V 6868-57 gibt es einige wesentliche Änderungen; so werden nun z. B. die Monitore nicht mehr einzeln betrachtet, sondern im Gesamtsystem zusammen mit der angeschlossenen Workstation und der verwendeten Software. Da die neue Norm seit ihrer Veröffentlichung einige Fragen aufgeworfen hat, soll dieser Technical Review die Stärken und Schwächen der neuen Norm aufzeigen. So sind z. B. die Einführung einer maximalen Beleuchtungsstärke oder die Verlängerung des Prüfindervalls von viertel- auf halbjährlich positiv zu sehen, während besonders die arbeitstägliche Konstanzprüfung zu Problemen führt und z. B. durch einen randomisierten Test ersetzt werden sollte. Daneben wird zusätzlich die medizinische Relevanz einiger Prüfpunkte hinterfragt sowie ein Überblick über die momentan angebotene Qualitätssicherungssoftware gegeben.

► **Table 1** Overview of abbreviations and terms.

Abbreviation	Term	Explanation
IDD	image display device	monitor
IDS	image display system	comprises the entire workstation with CPU, graphic card, software, and monitor(s)
E	Illuminance	describes the brightness in a room, unit: Lux (lx)
GSDf	Grayscale Standard Display Function	function which assigns luminance values which have been adapted to the non-linear contrast sensitivity of the human eye to the digital input signal
$L'_{\min}$	Minimum luminance	minimum luminance that a monitor can display (black). Includes ambient light. Unit: cd/m <sup>2</sup>
$L'_{\max}$	Maximum luminance	maximum luminance that a monitor can display (white). Includes ambient light. Unit: cd/m <sup>2</sup>
$L_{\text{amb}}$	Veiling glare	luminescence reflected onto the monitor by the ambient light. Unit: cd/m <sup>2</sup>
RC	Room class	Defines the requirements for luminance

## Introduction

The findings of digital X-ray images are to a considerable extent dependent on the quality of the monitors and the ambient conditions in the reading room. This dependence is only minor for clearly recognizable lesions with high contrast, as they can hardly be overlooked even under unfavorable conditions. This dependence, however, is critical with respect to lesions in the low-contrast range. Here, the highest quality criteria are required which are rarely met by standard PC components (monitor, display controller, etc.). The physician can only be assured by means of acceptance and constancy tests that the monitors meet these requirements at all times.

Nowadays flat screens are used almost exclusively (an overview of the abbreviations used are given in ► **Table 1**) instead of cathode ray tube monitors. This resulted in an urgent adaptation of the DIN standards for the acceptance and constancy testing of diagnostic monitors to the state of the art. Shortly after publication of the new standard, DIN 6868-157 [1], there was a comprehensive overview of these changes [2]. Nevertheless, since its publication, the standard has raised numerous questions and has led to many uncertainties among users. This has been made clear, for example, by the many questions in the online forum “Forum Röntgenverordnung” (a forum dealing with questions regarding the X-ray Ordinance, standards, etc.) [3]. This technical review deals critically with the new standard and describes initial experiences with DIN 6868-157 while providing help with the application of the standard. In doing so, the medical relevance of some test items is also scrutinized.

## Essential Changes to the previous Testing Procedures

A major change to the previous test situation is the consideration of the entire image display system (IDS) as a complete workstation with a PC, software and monitors, in contrast to an image display device (IDD). This standard has the advantage of requiring

that changes to all components that can influence image quality, such as the display controller, are also checked and documented, and not just the monitors themselves. ► **Fig. 1** shows, for example, the consequences of an incompatible display controller and the resulting difference in brightness between the upper and lower half of the monitor.

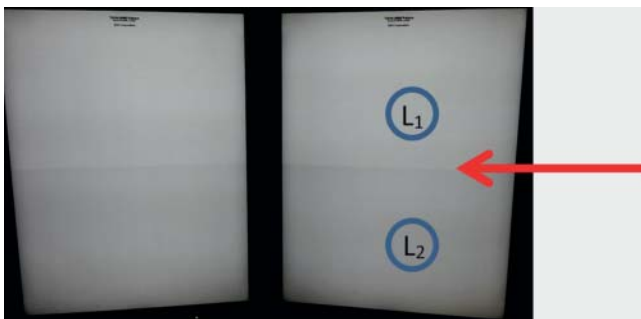
In addition to the image display system, the standard additionally includes the ambient lighting conditions. Previously they were implicitly checked by measuring the minimum luminance and veiling glare, whereas the new standard explicitly requires measurement of the illuminance of the room. The lighting is regulated by the newly-introduced room classes (RC). The room classes reflect various operating conditions of the monitors (► **Table 2**). The activities carried out in the room (diagnosis, examination, etc.) determine the room class and thus set the requirements for the maximum permitted illuminance and the monitor used. The earlier classification of projection radiography (thorax, skeleton, breast) into category A, and classification of fluoroscopy, computed tomography and subtraction angiography into category B have been omitted in their previous form.

In addition to the requirements for the acceptance test, the new standard also contains instructions and limiting values for the constancy test, which was previously regulated by the quality assurance guideline (QS-RL, Germ. Qualitätssicherungs-Richtlinie). In addition, the DICOM Grayscale Standard Display Function (GSDf) that adapts the luminance values to the sensitivity of the human eye for contrast changes is now mandatory for medical displays. Furthermore, contact measurement using a near-field luminance meter is now approved as an addition to the usual distance measurement in the telescope method for the constancy test and certain parts of the acceptance test. For the first time, limits for pixel defects were introduced. The standard is valid exclusively for application areas within the framework of the X-ray Ordinance, that is, not applicable to ultrasound equipment or MRI units.

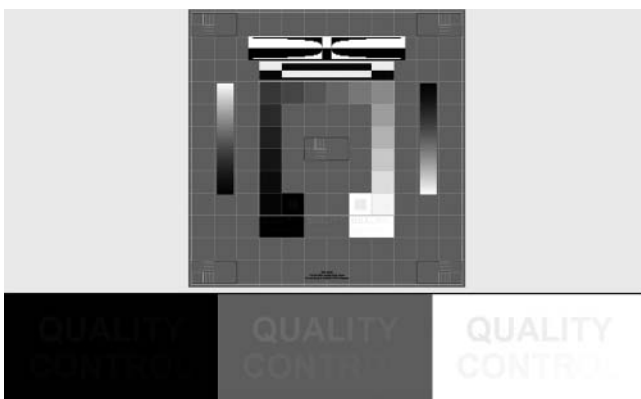
Modification of the quality assurance guideline resulted in the mandatory application of DIN 6868-157 dated December 15, 2014, thus replacing DIN V 6868-57 [4, 5]. However, old accep-

► **Table 2** DIN 6868-157 introduces a classification for different types of rooms, e.g. reading room, treatment room, etc. and defines the limiting values for the illuminance accordingly.

Room class	Room	Activities according to DIN 6868-157	Illuminance
RC1	reading room	evaluation of radiographs and projections	≤ 50 lx
RC2	examination room with immediate establishment of a diagnosis	medical activities in the examination room in which therapy-related decisions are made	≤ 100 lx
RC3	rooms for performing the examination	activities during which the examination is carried out using a dialog monitor	≤ 500 lx
RC4	observation and treatment rooms	activities in which a known and assessed diagnosis must be repetitively reproduced	≤ 1000 lx
RC5	dental diagnostic workstation	diagnosis outside the luminance requirements of a dental treatment room	≤ 100 lx
RC6	dental treatment room	diagnosis following the luminance requirements of a dental treatment room	≤ 1000 lx



► **Fig. 1** An incompatible display controller causing a difference in luminance. Luminance  $L_1 = 192 \text{ cd/m}^2$ ,  $L_2 = 184 \text{ cd/m}^2$  in test pattern TG18-UN80.



► **Fig. 2** Element 3 of the test pattern TG18-OIQ displays the letters “QUALITY CONTROL” in a black, a gray and a white rectangle.

does the new standard have to be applied. Likewise, constancy tests can continue to be performed according to QS-RL.

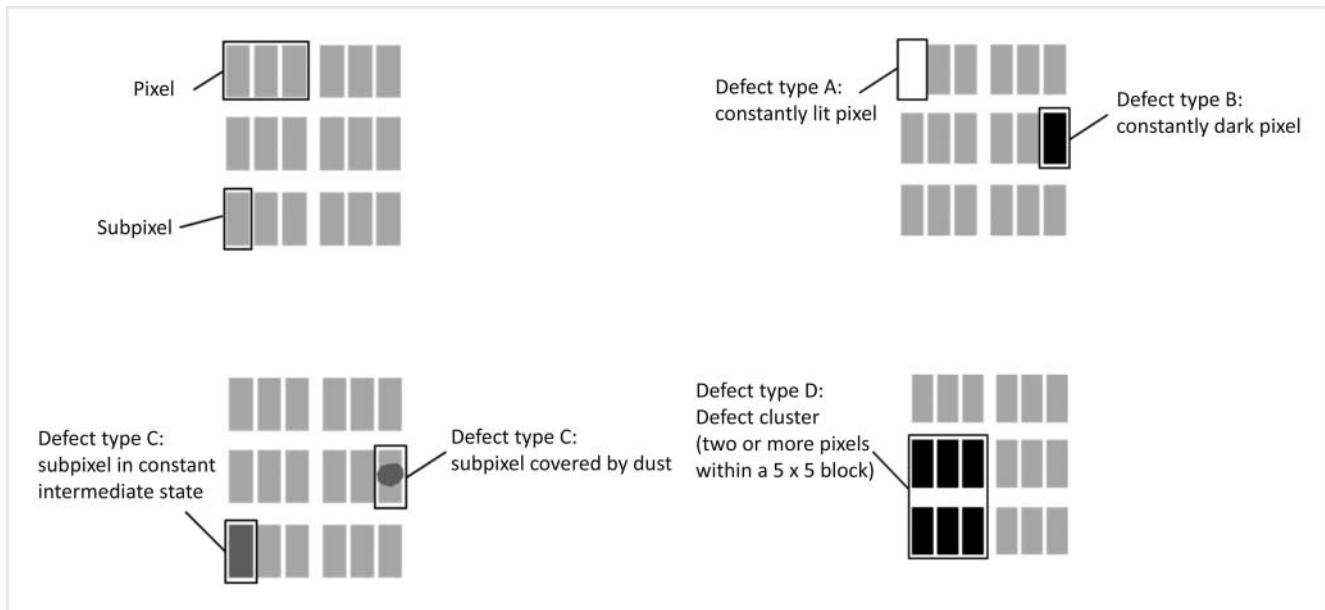
## Acceptance and Constancy Testing

As before, acceptance tests are necessary during commissioning as well as after monitor replacement. According to the new standard, an acceptance test must also be carried out if the room class changes. Only the radiation protection responsible/commissioner can change this if the relevant activities are modified. A constancy test is sufficient for a change of location. Regular constancy tests need only be carried out semi-annually instead of quarterly as before.

### Test Patterns

The patterns used for testing have been adapted to DIN EN 62563-1:2014-01; test patterns used for mammography have been supplemented by additional images of the American Association of Physicists in Medicine (AAPM) [6, 7]. These test patterns can be obtained in the standard  $1024 \times 1024$  pixel format as a bitmap via the Radiology Standards Committee (NAR, Germ. Normenausschuss Radiologie). Based on what we know so far, other storage formats such as DICOM or other resolutions, e.g.  $1600 \times 1200$ , which represent the minimum requirement for projection radiography are, unfortunately, not available so the user usually needs a software application containing the images required for acceptance and constancy testing. This can result in expenses in the amount of several hundred euros if the testing software is not included in the purchase of the monitors. These additional costs may be acceptable for an acceptance tester, but this will tend to lead to misunderstandings and reduced acceptance of the test by the operators (medical practices, etc.).

tance tests according to DIN V 6868-57 remain valid during a transitional period until 2025. This also includes an exchange of subcomponents, e.g. the PC; only after replacing the monitors



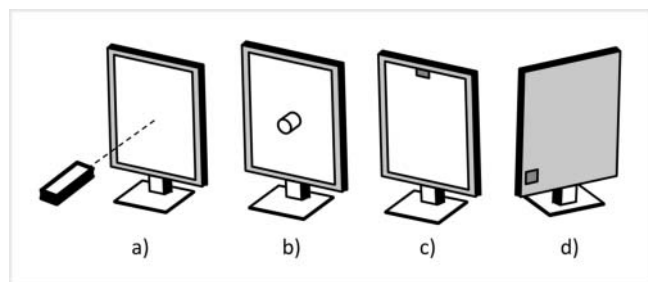
► **Fig. 3** Display of pixels and subpixels on a gray-scale monitor and possible defects. In a color monitor, a pixel is composed of one red, one green and one blue subpixel. Different colors can be displayed by combining these subpixels. The arrangement of these subpixels can differ, depending on the manufacturer.

## Visual Inspections

### Overall Image Quality

The newly introduced test pattern TG18-OIQ (overall image quality) is used to assess the overall image quality and geometry during the acceptance test as well as the daily constancy test (► **Fig. 2**). Various test image elements have to be assessed depending on the room class. The greatest challenge is test element 3, which shows the lettering “QUALITY CONTROL” in low contrast on white, gray and black fields. From left to right the individual characters are displayed in decreasing contrast. Depending on the room and application class, different characters of the lettering must be visible. The highest requirements apply to mammography, where the entire lettering must be recognizable. At 12 bits, the final letter “L” in the black field corresponds to a pixel value of 16, which corresponds to just 0.4% of the maximum gray scale value. Previously only the 5% field had to be recognizable (corresponds roughly to the “U” in “QUALITY”). It is not clear why these requirements were so significantly raised. Thus, for example, EUREF (European Reference Organisation for Quality Assured Breast Screening and Diagnostic Services) does not require legibility of the entire lettering, but that the number of observed characters remains constant [8]. The contrast of the lettering is so low that the other test image elements can influence the evaluation of the test item. This is easy to check by covering the areas around the black field so as not to dazzle the eye.

The value and acceptance of the currently valid procedure was examined in a blind study. To do this, over a period of six weeks the study determined how often and with what care the daily constancy tests were performed. Four modified versions of the TG18-OIQ test image were developed in which either characters in the



► **Fig. 4** Methods for measuring the luminance: **a** telescope method, **b** near range luminance meter, **c** front integrated luminance meter, **d** back integrated luminance meter. Methods **b–d** require an additional measurement of the illuminance.

“QUALITY CONTROL” lettering or the line pair grids in the corners and center were removed. The modified test patterns were included into the RadiCS quality assurance software made by EIZO and, unknown to the users, remotely controlled distributed daily to five to ten diagnostic workstations via a server. A total of 616 tests were evaluated, of which 172 (28%) used modified test patterns. The completion rate during the testing period was 88%. This means that 12% of all pending examinations were aborted or skipped by the examining physician. Of a total of 148 valid tests with modified test images, only 7 (5%) were correctly recognized as faulty. In 141 cases (95%), however, the test was incorrectly rated as passed. Subsequently, the users were informed about the study, and a second phase examined whether this could lead to a change in the performance of the constancy test. Modified test images were distributed over a shortened two-week test period. A total of 276 examinations were evaluated, of which 29 used modified images. The completion rate was 85% and could

not be increased. Of a total of 25 tests with modified test images, 7 (28%) were correctly classified as faulty, whereas 18 (72%) were mistakenly considered to be passed. This shows, on the one hand, the lack of acceptance of the constancy tests and on the other hand, the low significance of the test results.

Overall, the daily constancy test according to the new standard is considerably more extensive than before. Whereas previously only a check of gray-scale reproduction was prescribed, the overall picture quality is now to be checked visually by means of several elements of the TG18-OIQ test image. The additional workload reduces the acceptance of the test by the user, but there is no evidence of any additional benefit.

### Homogeneity, Color Impression and Uniformity, Defective Pixels

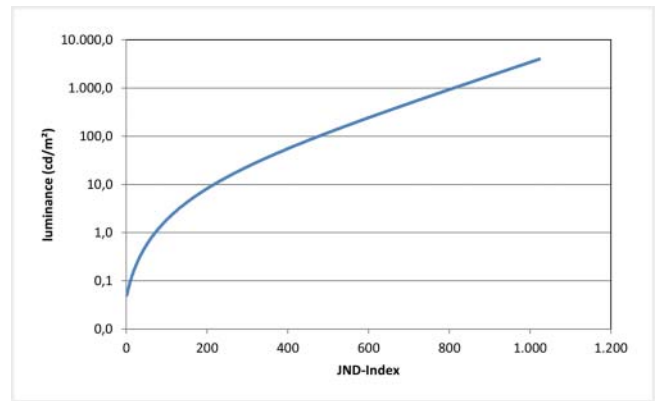
In both the acceptance and constancy tests, the monitors must be tested for homogeneity and color impression using the TG18-UN80 test pattern (uniformity, at 80% of the driving level). A check for dead pixels is strictly required only in the acceptance test, but should also be checked in the constancy test.

Previously it was required that the medically used area of the display device must not contain artifacts which influence the diagnosis. Artifacts can be caused by defective pixels, among other things. An accurate assessment of when these pixel defects affect the diagnosis is difficult to determine and also varies with the person carrying out the test, therefore the new standard has defined several types of pixel defects and sets limiting values. A distinction is made among permanently lit pixels (defect type A), permanently dark pixels (defect type B), abnormal subpixels which do not correspond to error types A or B (defect type C) and defect clusters (defect type D), see ► Fig. 3. The exact number of allowed pixel defects must be calculated based on the specified limits for a resolution of 1024 × 1024 and total number of pixels of the image display. It may be helpful for the examiner to create a table with the limiting values of the most frequent resolutions if the software does not provide such a calculation.

A typical display device for mammography with a resolution of 2048 × 2560 may have 5 pixel errors of defect type A, 25 type B defects, 25 type C defects, and 5 type D pixel defects, thus a total of 180 defective (sub)pixels. Especially when combining several – or in the extreme case all four – defect types, these limiting values appear to be too high. In practice, working with so many pixel defects is hardly imaginable and would be rejected by most physicians.

### Measurement Testing

As in the past, the acceptance test is carried out as a distance measurement using the telescope method (measurement method A), but other methods can also be used in the constancy test (► Fig. 4). The standard permits the use of the calibrated luminance meter according to the telescope principle of the acceptance test as well as the near range luminance meter for contact measurement (method B), as well as meters integrated into the image display system (method C + D). In test procedures B, C and D, the illuminance must also be determined in order to account for the ambient light. With a suitable software, the



► Fig. 5 The grayscale standard display function shows the changes in luminance that are necessary for a human observer to notice a difference (“just noticeable difference”, JND). The luminance response of the display will be adjusted accordingly.

constancy test can be carried out automatically and, depending on the software, in some cases even remotely controlled.

### Illuminance

An addition to DIN 6868-157 was the requirement that the illuminance must be adapted to the environment. Requirements for the maximum illuminance are determined by the room class.

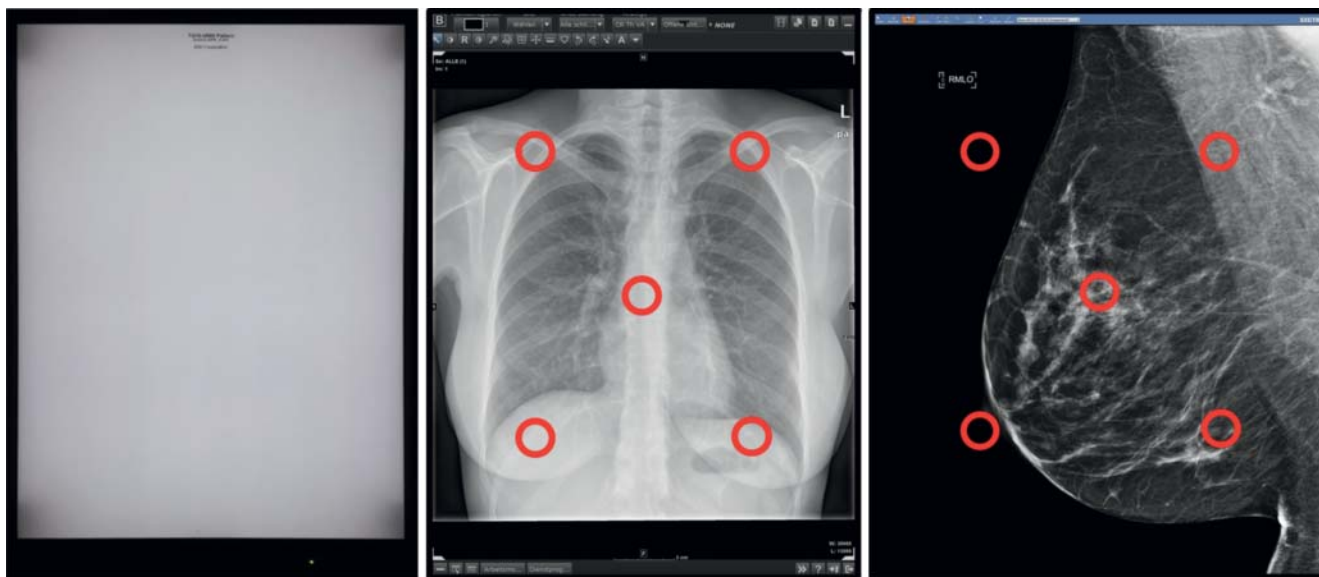
### Minimum/Maximum/Veiling Glare

The minimum and maximum luminance must be measured for the constancy tests. The ratio of minimum and maximum luminance (maximum luminance ratio, formerly maximum contrast) has to be determined only in the acceptance test. Absolute limits for the maximum luminance and maximum luminance ratio are specified depending the application. The minimum requirements for the maximum luminance ratio were raised from 100 to 250 for projection radiography and from 40 to 100 for other application areas. The transitional periods for legacy equipment will lead to a difference in quality between old and new monitors in the coming years.

### Luminance Response

In order to accommodate the nonlinear contrast sensitivity of the human eye, the new standard made the grayscale standard display function obligatory for display devices with diagnostic quality (► Fig. 5). The human eye is more sensitive to minor relative changes in areas of higher luminance (white) compared with low-luminance areas (black). The introduction of a standard luminance response results in a comparable image impression on different monitors, even among different manufacturers.

The luminance response is determined with contact measurement at the 0 – 100% driving levels (test images TG18-LN8-01 to 18). A suitable software tool is necessary for the evaluation of the measured values. If no quality assurance software is used, the tool offered by the European Reference Organization for Quality Assisted Breast Screening and Diagnostic Services (EUREF), for exam-



► **Fig. 6** Left: The test pattern TG18-UN80 shows shaded edges as a typical sign of ageing. The display passes the constancy test. Right: The part of the display that is used for reading varies with the anatomical region (e. g. chest, breast) and the application software (e. g. PACS).

ple, can be used [10]. Veiling glare  $L_{amb}$  has to be considered in the calculations since contact measurement is prescribed.

Exceptions were applications in dentistry (RK5 + 6), in which the GSDF is not mandatory, since low contrasts play only a subordinate role in dentistry. In room class 3 the GSDF has to be measured only in the acceptance test.

### Display Homogeneity

In order to guarantee that the image impression is uniform across the entire monitor, the homogeneity of the display system must be measured at fixed points at 10% and 80% of the maximum digital driving level during the acceptance test. The number of measuring points depends on the screen diagonal and thus also takes into account large monitors that replace two smaller individual monitors (e. g. one 6 MP monitor instead of two 3 MP monitors).

According to the old standard, different test patterns could be used for checking homogeneity, but it was prescribed that one measuring point should be placed near each of the four corners. Following the new definition, the measuring points were moved further towards the center; a check of the corners or edge is thus no longer performed. Although only the medically used area of an imaging display is supposed to be checked and not the area which is concealed, by the menu bar of the PACS, for example, inhomogeneity tends to appear along the edge and corners, and not in the area to be checked according to the standard (► Fig. 6). The larger the monitor, the further removed the measuring points are from the edge. It would therefore be advisable to carry out the measurements at a certain distance from the edge of the medically used area regardless of the monitor size.

A further modification concerns the definition of homogeneity. Previously, the deviation of the vertices (E1 – 4) from the center (M1) was considered, whereas now the deviation of the measuring point with the highest luminance to the point with

the lowest luminance is evaluated. At the same time, the tolerances were adapted to this changed approach. According to the old standard tolerances of  $\pm 15\%$  (application category A) or  $\pm 20\%$  (application category B) were used for the deviation of luminance of the vertices from the center. Now, the limiting value for homogeneity within the entire display device is 25% (RK1 – 4) and 30% (RK5 + 6). ■Because of this revised approach monitors■ which do not meet the requirements of the prior standard may be operated according to the new standard. According to the old standard, a monitor with  $171 \text{ cd/m}^2$  in the center (M1, z) and  $135 \text{ cd/m}^2$  in one of the corners (E1,  $k_1$ ), exhibits a deviation of approx. 21% thus exceeds the tolerances for application categories A and B display devices. According to the new standard, homogeneity is approx. 24%, thus fulfilling requirements for all applications. Therefore, the monitor in ► Fig. 6 would pass the measurement tests of the new standard on the one hand due to the position of the measuring points and on the other hand due to the changed limiting values. In the case of a visual complaint by the user, this may lead to discussions regarding warranty claims.

### Multi-display Image Homogeneity

The check of the homogeneity of adjacent monitors connected to the same image display system and which are supposed to show an identical image was also introduced. This is a positive step, since a workstation frequently consists of several monitors, and varying image impressions should be avoided. A similar rule already existed for mammography in PAS 1054 [11], according to which maximum contrast and maximum luminance were compared. In the new standard, homogeneity of multiple display systems is measured at low luminance (10% of the maximum driving level, test image TG18-UN10). A comparison of the whole luminescence response would be more useful instead. It remains to be seen how these changes will affect mammography. For other acquisition methods for which there were no requirements

► **Table 3** The authors recommend the following limiting values for constancy tests according to DIN 6868-157.

test	interval	method	test image	limiting value	tolerance
overall image quality	daily	visually	TG18-OIQ or TG18-QC	<ul style="list-style-type: none"> <li>▪ line pair–grid visibility</li> <li>▪ visibility of 5% and 95% fields (only dentistry)</li> <li>▪ visibility of characters “QUALITY CONTROL” in white and gray field (dentistry in gray field only)</li> <li>▪ visibility of characters “QUALITY CONTROL” in black field:               <ul style="list-style-type: none"> <li>▪ RC1 (mammography) QUALITY CONTROL</li> <li>▪ RC1 except mammography: QUALITY CONTRO</li> <li>▪ RC2 QUALITY CONT</li> <li>▪ RC3 QUALITY CON</li> </ul> </li> <li>▪ entire visibility of grid</li> <li>▪ continuity of ramp bar</li> </ul>	–
homogeneity of luminescence	semi-annually	visually	TG18-UN80	no interfering irregularities	–
color impression and uniformity	semi-annually	visually	TG18-UN80	<ul style="list-style-type: none"> <li>▪ Color uniformity across the screen</li> <li>▪ Color uniformity across multiple displays</li> </ul>	–
minimum luminance ( $L_{\min}$ )	semi-annually	metrologically	TG18-LN8 – 01	$\geq 1.1 L_{\text{amb}}$ (1.1 times veiling luminance)	reference value $\pm 30\%$
maximum luminance ( $L_{\max}$ )	semi-annually	metrologically	TG18-LN8 – 18	<ul style="list-style-type: none"> <li>▪ projection radiography, mammography: <math>\geq 250 \text{ cd/m}^2</math></li> <li>▪ fluoroscopy, computed tomography: <math>\geq 150 \text{ cd/m}^2</math></li> <li>▪ mammographic stereotaxy, RK5: <math>\geq 200 \text{ cd/m}^2</math></li> <li>▪ RK6: <math>\geq 300 \text{ cd/m}^2</math></li> </ul>	reference value $\pm 30\%$
veiling glare ( $L_{\text{amb}}$ )	in case of abnormalities of minimum luminance: semi-annually	metrologically	–	–	reference value $\pm 30\%$ (exception: reference value $< 0.15 \text{ cd/m}^2$ , then reference value $+ 30\%$ )
illuminance (E) (alternative to veiling glare)	semi-annually	metrologically	–	<ul style="list-style-type: none"> <li>▪ RC1: <math>E \leq 50 \text{ lx}</math></li> <li>▪ RC2: <math>E \leq 100 \text{ lx}</math></li> <li>▪ RC3: <math>E \leq 500 \text{ lx}</math></li> <li>▪ RC4: <math>E \leq 1000 \text{ lx}</math></li> <li>▪ RC5: <math>E \leq 100 \text{ lx}</math></li> <li>▪ RC6: <math>E \leq 1000 \text{ lx}</math></li> </ul>	–

▶ **Table 3** (Continuation)

test	interval	method	test image	limiting value	tolerance
homogeneity (H) of multiple display units	semi-annually	metrologically	TG18-LN10	-	<ul style="list-style-type: none"> <li>■ mammography: H &lt; 10 %</li> <li>■ projection radiography, fluoroscopy, computed tomography, mammographic stereotaxy: H &lt; 20 %</li> <li>■ dentistry: H &lt; 30 %</li> </ul>
luminescence response	semi-annually	metrologically	18 test images TG18-LN8-01 through TG18-LN8-18	-	<ul style="list-style-type: none"> <li>■ Projection radiography, mammography: GSDF ± 10 %</li> <li>■ Fluoroscopy, computed tomography: GSDF ± 15 %</li> </ul>

regarding the homogeneity of multiple display systems the introduction of this test item represents a tightening of the rules.

### Limiting Values and Tolerances for the Constancy Test

For constancy tests, DIN 6868-157 specifies both absolute limits as well as tolerances for deviation from the reference values. Since it is not useful to use limit values and tolerances for each test item, and since a general listing is missing in the standard, ▶ **Table 3** contains the limiting values and tolerances which, in the authors' opinion, should be used according to the new standard.

## Quality Assurance Software

In principle, it is possible to carry out acceptance and constancy tests without quality assurance software. Since the DIN test images are available only in the standard 1024 × 1024 format, a software solution is usually required to generate the test images at other resolutions. Furthermore, testing is simplified if the related test images are immediately called up and the results documented.

Quality assurance software is provided by manufacturers of diagnostic monitors (e. g. Barco, EIZO), measuring equipment (iba) or PACS (aycan), but also by quality assurance service providers (diraal, mdp dental). ▶ **Table 4** shows an overview of currently available quality assurance software focused on DIN 6868-157.

The scope of functions available differs distinctly. For example, software by mdp dental is designed only for dentistry, while other programs cover all areas of application. Depending on the manufacturer, the software is often modularly constructed, so that in the basic version, for example, only the constancy test is available which is sufficient for most users, thus keeping costs down.

Some manufacturers also offer the option to save the results of the acceptance and constancy tests centrally on a server. This can be particularly useful for larger hospitals or multiple-site practices in order to quickly access protocols. A server solution is generally not required for single workstations.

Prices of quality assurance software vary substantially. Some manufacturers offer software at no cost together with the purchase of other products, such as diagnostic monitors; with other manufacturers, on the other hand, a few hundred euros have to be invested in addition to the cost of the workstation. Therefore, prior to purchasing software the requirements should be carefully considered to avoid unnecessary costs.

## Discussion

An adaptation of the standard to the state of the art is in principle to be welcomed. In addition to some improvements, such as the extension of the test interval from quarterly to semi-annual tests, several items of DIN 6868-157 must be seen critically. Particular attention is to be paid to the daily constancy test.

Acceptance of this test among physicians is low. This is primarily due to the tests requiring the user to only confirm the visibility in a permanently identical test pattern, thus calling into question the usefulness of this exercise. Randomized tests in which the



► **Table 4** Overview of available software for quality control according to DIN 6868-157.

manufacturer	software	central storage of protocols?	miscellaneous
AYCAN	ayDisplayQuality Software	archiving in PACS	plug-in for aycan OsiriX PRO
barco	QA Web for DIN 6868 – 157	server	
diraal	QAXRAY Pro	server	
EIZO	RadiCS	server	
goFileMaker	gFM-dental	database	dentistry only
iba	DisplayQ	no	modular; documentation and display of test images separate
mdp dental	KPS 2015	no	dentistry only; modular
NEC	GammaCompMD QA	server	cooperation with diraal
Qubyx	PerfectLum	server	

user has to recognize a structure at any point on the screen and subsequently point to it with the mouse are much closer to the actual diagnostic situation. These tests also directly provide a convincing result in which the physician is assured that the monitor together with the ambient lighting conditions have a high probability of meeting quality requirements.

When evaluating the test point, a bias is generated as the user knows exactly what should be seen, thus deviations from the standard may not be recognized for an extended period of time. In this case as well, a randomized test, in which not only the objects to be recognized but also their positions vary from test to test and must be recognized by the tester, would be advantageous. In this way a subjective test would become a semi-objective test. Possibly, these semi-objective tests could even replace the metrological checks, which would lead to a cost reduction. There are already similar approaches, such as the Moni-QA software program [9].

In addition to the daily visual constancy test, metrological verification of homogeneity should be seen in a critical light. On the one hand, the threshold has been raised; on the other, the newly-defined measuring points are placed too far in the center of the monitor. Inhomogeneity in the outer regions of the screen is thereby not detected. It would therefore be more advantageous to carry out the measurements at a strictly defined short distance from the edge of the medically used area.

The standard includes limits for pixel defects, providing a clear benchmark for the manufacturer, examiner and user. Previously there was a subjective estimate of the number of allowable pixel defects, which could lead to different opinions, especially between manufacturers and users. While the introduction of limiting values is therefore generally to be assessed positively, the thresholds themselves have been poorly chosen, however. The limits are clearly too high, particularly when combining several types of defects.

The new standard also allows built-in sensors and automated measurements for the tests. The quality assurance software of one manufacturer supports the remote performance of the semi-annual test without a trained inspector on-site. However it

is not advisable to allow a completely remote-controlled test in which the device checks itself. In recent months numerous discussions have shown the dubiousness of device-internal testing software (e. g. the emissions scandal at VW).

Quality assurance of diagnostic monitors must not only be aimed at checking compliance with physical parameters, especially since the correlation of these parameters with the needs of radiological activities has not always been proven. Rather, quality assurance must demonstrate that the processing of a binary image is optimally adapted to human visual physiology under the given ambient conditions. For this reason, the eye of the user must absolutely be included in the test.

## Summary

The transition of image displays from cathode ray tubes to systems using flat screen monitors made an adaptation of the standard to the state of the art urgently necessary. The new standard has led to some improvements, but many questions have been raised by the users as a result of standard's complexity.

Likewise, the integration of dental applications into the standard was only partially successful. In many aspects exceptions for dentistry resulted in a considerably reduced range of testing.

On the whole, the new standard contains numerous exceptions that make understanding and interpretation difficult. Compared with the earlier standard, requirements were increased for many test items, such as visibility of low contrast in the daily constancy test. Other items, such as homogeneity requirements, were lowered.

The clash of interests during the creation of the standard has been made clear by the numerous objections to the drafts. However, the resulting compromise has led to further discussions and criticism since the publication of DIN 6868-157. A revision of the standard to eliminate ambiguities is therefore to be welcomed; especially useful would be the introduction of randomized tests.

**CLINICAL RELEVANCE**

- The physician has to be confident that the diagnostic monitor can display all relevant lesions,
- therefore regular monitor testing is indispensable.
- Since November 2014, DIN 6868-157 has governed the acceptance and constancy testing of diagnostic monitors.
- Numerous users are having problems implementing the new standard.
- A revision of the standard to clarify misunderstandings appears necessary.
- Randomized tests should be used for daily constancy testing.

**Conflict of Interest**

The authors declare that they have no conflict of interest.

**References**

- [1] Normenausschuss Radiologie (NAR) DIN 6868-157. Sicherung der Bildqualität in röntgendiagnostischen Betrieben – Teil 157: Abnahme- und Konstanzprüfung nach RÖV an Bildwiedergabegeräten in ihrer Umgebung. November 2014
- [2] Madsack B, Walz M, Weisser G. Abnahme und Konstanzprüfung an Bildwiedergabesystemen. *Radiopraxis* 2014; 7: 195–210
- [3] Forum-Röntgenverordnung. <http://www.forum-roev.de/forum.php> Stand: 04.11.2016
- [4] Qualitätssicherungs-Richtlinie (QS-RL) zur Durchführung der Qualitätssicherung bei Röntgeneinrichtungen zur Untersuchung oder Behandlung von Menschen nach den §§ 16 und 17 der Röntgenverordnung.
- [5] Normenausschuss Radiologie (NAR) DIN 6868-57. Sicherung der Bildqualität in röntgendiagnostischen Betrieben Teil 57: Abnahmeprüfung an Bildwiedergabegeräten. Februar 2001
- [6] Normenausschuss Radiologie (NAR) DIN EN 62563-1. Medizinische elektrische Geräte – Medizinische Bildwiedergabesysteme – Teil 1: Bewertungsmethoden. Januar 2014
- [7] American Association of Physicists in Medicine (AAPM) Task Group 18. Report No. 03: Assessment of Medical Display Performance for Medical Imaging Systems. April 2005
- [8] Perry N, Broeders M, de Wolf C et al. European guidelines for quality assurance in breast cancer screening and diagnosis. 2006; 4th Edition
- [9] Jacobs J, Rogge F, Kotre J et al. Preliminary validation of a new variable pattern for daily quality assurance of medical image display devices. *Med Phys* 2007; 34: 2744–2758
- [10] LRCB. Monitor Check. <http://www.euref.org/downloads> Stand: 04.11.2016
- [11] Blendl C, Hermann KP, Mertelmeier T. Anforderungen und Prüfverfahren für digitale Mammographie-Einrichtungen PAS 1054. Beuth Verlag. 2005