Introduction

Ultrasonography (US) is the preferred and widely accepted first choice imaging modality for the evaluation of testicular abnormalities [1]. B-mode US has a very high sensitivity when investigating the scrotum. Furthermore, new additions to B-mode US such as color Doppler, contrast-enhanced ultrasound, and recently elastography have been developed over time [2]. Elastography is a noninvasive method to evaluate tissue stiffness [3], which can be assessed by either strain or shear wave. Strain elastography uses external transducer compression and continuously compresses the tissue of interest [4], whereas shear wave is a quantitative method [5–7]. Since lesions in testicles are superficial, both elastography methods could be used. However, elastography should be recommended as part of a multiparametric ultrasound examination approach, also suggested by Sidhu [8].

Comparison of Tissue Stiffness Using Shear Wave Elastography in Men with Normal Testicular Tissue, Testicular Microlithiasis and Testicular Cancer

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ABSTRACT

Objectives  To compare elastography measurements in men with normal testicular tissue, testicular microlithiasis and testicular cancer.

Methods  A total of 248 consecutive patients were included. All men provided written informed consent. Testicular stiffness was assessed using shear wave elastography (SWE). Three SWE velocity measurements were assessed in each testicle. The patients were divided into three groups; men with normal testicular tissue (n = 130), men with testicular microlithiasis (n = 99) and men with testicular cancer (n = 19).

Results  We found a higher mean velocity in the group of patients with testicular cancer (1.92 m/s (95 % CI 1.82–2.03)) compared to both the group with normal tissue (0.76 m/s (95 % CI: 0.75–0.78)) (p < 0.001) and the group with testicular microlithiasis 0.79 m/s (95 % CI: 0.77–0.81) (p < 0.001).

Conclusion  The presence of testicular microlithiasis increased stiffness slightly, but within the range of variation in normal testicles. Increased stiffness may indicate testicular malignancy in testicular lesions. Ultrasound elastography could be a very useful tool when investigating scrotum.
Elastography is used in various organs [7, 9–11] and also in the testicles for investigating testicular torsion [12, 13], testicular cancer [14, 15], infarction [16, 17], epidermoid cysts [18], undescended testes [19], infertile men [20], hemodialysis patients [21], testicular microlithiasis, and other lesions [22–24]. It can be challenging to distinguish hard tumors in soft tissue using only B-mode ultrasound. Therefore, elastography is instrumental in differentiating normal from pathological tissue [5]. In an elasticity phantom comparing strain and shear wave elastography, Carlsen et al. [25] showed that the two methods were equally applicable in intermediate levels of elasticity, but strain was better in hard and soft targets.

The aim of this study was to compare shear wave elastography (SWE) in patients with normal testicular tissue, TML, and testicular cancer.

**Materials and Methods**

**Study population**

A total of 248 consecutive patients from the Department of Radiology were included during the period between September 2013 and March 2016. All included patients were outpatients referred by their general practitioner for a clinical US scrotal examination due to symptoms such as pain, discomfort, lump or testicular mass. The exclusion criteria were torsion, inflammation, previously diagnosed testicular cancer, an age of less than 18 years or any linguistic difficulties regarding understanding of the informed consent. The patients were divided into three groups: normal testicular tissue, TML, and testicular cancer.

**Elastography image technique**

All patients underwent B-mode US investigation followed by SWE. In order to avoid signal artifacts, care was taken not to compress the testicle during the elastography investigation. SRR, MRP, or one of four certified radiologists (all had more than five years of ultrasound experience and between six months to 5 years of elastography experience) performed the SWE measurements. First a B-mode investigation was performed followed by SWE. All examinations were performed separately for the right and left testicle and on the same ultrasound machine. The three SWE measurements were performed in the center, upper and lower pole. In patients with testicular cancer, the three SWE measurements were performed in the center, upper and lower pole of the lesion. If an elastography measurement error occurred, a new measurement was performed within seconds. We used a 9 MHz linear 9L4 probe for all examinations (Siemens S3000 ultrasound machine (Acuson Corporation, Siemens, Mountain View, CA, USA) with Virtual TouchTM Tissue Quantification software). The frame rate per second (frs) was 14; the thermal index for soft tissue (TIS) was 0.8; the thermal index for bone (TIB) was 1.2; and the mechanical index was 1.6. A detection pulse measured the speed of the shear waves, and the shear wave velocity was quantified in meters per second from the region of interest (ROI). A B-mode image was used to place the ROI in order to perform elastography. The ROI size was a 10 × 10 mm box, which could not be altered. Three shear wave velocity measurements were performed in each testicle with the patient in the supine position. The SWE results are presented in meters per second (m/s). All images and data were recorded in the Picture Archive Communication System (PACS, Easyvizi Impax Workstation, Medical Insight, Valby, Denmark). Elastography is easily performed without discomfort or pain to the patient.

**Statistical analysis**

We estimated the mean testicular tissue stiffness in the three groups of men using a linear mixed effects model to account for the cluster structure and estimated random variation. Data constituted a hierarchy of clusters of correlated observations: multiple measurements performed on the same testicle have a higher similarity than in comparison with those performed on the contralateral testicles. Likewise, the measurements in the same man are expected to be more similar than if compared with those performed in other men. Using the linear mixed effects model, it is possible to take random variation into account that can be attributed to heterogeneity between men, and also between testicles in the estimated elastography values.

Age and TML were adjusted for in the analysis, but neither was significant in the linear mixed effects model and hence were removed from the model. The linear mixed effects model was tested for normality by qnorm-plots of the residuals, and showed no cause of four certified radiologists (all had more than five years of ultrasound experience and between six months to 5 years of elastography experience) performed the SWE measurements. First a B-mode investigation was performed followed by SWE. All examinations were performed separately for the right and left testicle and on the same ultrasound machine. The three SWE measurements were performed in the center, upper and lower pole. In patients with testicular cancer, the three SWE measurements were performed in the center, upper and lower pole of the lesion. If an elastography measurement error occurred, a new measurement was performed within seconds. We used a 9 MHz linear 9L4 probe for all examinations (Siemens S3000 ultrasound machine (Acuson Corporation, Siemens, Mountain View, CA, USA) with Virtual TouchTM Tissue Quantification software). The frame rate per second (frs) was 14; the thermal index for soft tissue (TIS) was 0.8; the thermal index for bone (TIB) was 1.2; and the mechanical index was 1.6. A detection pulse measured the speed of the shear waves, and the shear wave velocity was quantified in meters per second from the region of interest (ROI). A B-mode image was used to place the ROI in order to perform elastography. The ROI size was a 10 × 10 mm box, which could not be altered. Three shear wave velocity measurements were performed in each testicle with the patient in the supine position. The SWE results are presented in meters per second (m/s). All images and data were recorded in the Picture Archive Communication System (PACS, Easyvizi Impax Workstation, Medical Insight, Valby, Denmark). Elastography is easily performed without discomfort or pain to the patient.
for concern. The proportions of random variation attributed to inhomogeneity between men and between testicles (within each man), and measurement error stemming from triple measurements on each testicle was estimated.

A p-value ≤ 0.05 was considered statistically significant. STATA statistical software (version 14.1, STATA Corporation, College Station, TX, USA) was used for the analysis.

Ethics and approvals
The Danish Data Protection Agency and The Regional Scientific Ethical Committees for Southern Denmark (ID: S-20120144) approved the study. All patients signed an informed consent after receiving both oral and written information.

Results
We included 248 consecutive patients with a total of 492 testicles (246 right testicles (146 (59.3 %) normal tissue, 90 (36.6 %) TML, 10 (4.1 %) cancers) and 246 left testicles (159 (64.6 %) normal tissue, 78 (31.7 %) TML, 9 (3.7 %) cancers). One of the 19 patients with testicular cancer had bilateral cancer.

The mean age in men with normal testicular tissue was 47.6 (range: 20–79 years), and in men with TML and testicular cancer it was 47.3 (19–94 years) and 39.7 (25–79 years), respectively.

We found a statistically significantly higher estimated mean velocity in the testicular cancer group compared to men with normal testicular tissue and TML (p < 0.001). Also, men with TML had a higher estimated mean velocity compared to men with normal tissue: 0.79 m/s vs. 0.76 m/s (p = 0.027) (Table 1).

In the group of patients with testicular cancer, the unaffected testicle had an observed mean value of 0.77 m/s. In men with unilateral TML, the observed mean of the unaffected testicle (without TML) was 0.81 m/s. The estimated elastography findings in the three groups of men are summarized in Table 1. Table 2 shows the estimated means from the three groups using the linear mixed effects model.

Nine testicles with cancer were diagnosed with seminoma and 10 testicles with non-seminoma. TML was present in one patient with non-seminoma and in four with seminoma. The tumors had a mean diameter of 3.6 cm (range: 0.6–8.2 cm) Fig. 1–4.
Discussion

Main findings

We found a higher estimated statistically significant stiffness in patients with testicular cancer compared to men with normal tissue. Additionally, the stiffness in men with TML was higher than in men with normal tissue. This difference, however, is considered too small to have any clinical relevance.

Comparison with other studies

A study of thyroid nodules showed that the presence of calcifications significantly increased the stiffness [26]. We also found men with TML to have increased stiffness compared to men with normal tissue ($p = 0.027$). In our study heterogeneity between testicles belonging to the same man was responsible for nearly two-thirds of random variation (62 %), but measurement error (35 %) and heterogeneity between testicles (3 %) also mattered. Although the difference in stiffness between testicles with normal tissue and TML was statistically significant, it was very modest and unlikely to be of clinical importance. An explanation may be the deposition of microlcalfications throughout the testicle, as also in the thyroid gland [26]. This consideration is also shared in the recently published guidelines on TML management, recommending that a limited group of men with risk factors be offered US follow-up, since epidemiological studies and recent reports do not consider TML to be premalignant [27].

Overall, the observed mean velocity in men with testicular cancer was 2.10 m/s, but we found a calculated predicted mean of 1.92 m/s. Trottmann et al. investigated seven patients with germ cell tumors and five with seminoma using virtual touch imaging quantification (VTIQ), and the results were a mean shear wave velocity of 1.94 m/s in germ cell tumors and 2.42 m/s in seminoma [22]. Macron et al. investigated the testes of 20 healthy patients using SWE and found a mean SWE of 0.81 m/s and a mean VTIQ of 1.07 m/s [28]. VTIQ seems to measure the stiffness higher than SWE, which could be caused by the very small ROI of the VTIQ. Both studies had small sample sizes and did not take random effects into account. Variation could also be related to the ultrasound machine, transducer, and software being used. Trottmann et al. also showed a statistically significant difference between mean shear wave velocity in normal testicular tissue (1.17 m/s), seminomas (2.42 m/s)
and germ cell tumors (1.94 m/s) \(p = 0.002\) \([22]\). An explanation for the observed velocity of 1.17 m/s in normal testicular tissue compared to our estimated mean of 0.76 m/s could be different elastography ultrasound machines. Another study \([29]\) investigated 60 healthy males and found velocities at the center of the testicle to be significantly lower (0.90 m/s) than the mean velocities of 1.15 m/s in the inferior and superior parts of the testicles, respectively \((p < 0.001)\). Whether this applies to testicular tumor tissue remains unknown.

Shin et al. compared shear wave velocities between different ultrasound machines and transducers in a phantom and found the difference in mean shear wave velocities between three machines to be statistically significant \((p \leq 0.002)\) \([30]\). This implies that caution is needed when using absolute cut-off values in the comparison of measurements from different ultrasound machines or transducers.

The main strengths of this study are the large number of patients and the inclusion of random variation in the data analysis. However, using random variation requires caution in the comparison of estimated results with observed results. We consider the use of SWE to be an asset, since it does not use manual transducer compression and therefore the testicular tissue is not displaced during measurement. Hence, SWE is operator-independent. The main limitation of this single center study is that it was only possible to obtain three velocity measurements in each testicle due to the daily workflow in our radiology department. More measurements would have yielded more precise estimates. This was also confirmed by our linear mixed effects model, which showed that increasing the number of measurements rather than the number of patients would increase the precision of the mean velocity from the three groups. Another limitation may be the relatively small number of patients with testicular malignancy \((n = 19)\) included in the study. However, the mean diameter of the tumors was large in our study population, and the ROI could easily fit most lesions. Further studies including a higher number of patients with testicular lesions are warranted.

In conclusion, our study shows that the presence of TML increases stiffness slightly, but the range is still within that of normal testicles. Increased velocity may indicate testicular malignancy in testicular lesions, and the use of elastography seems a promising method for the evaluation of testicular lesions.

Acknowledgements

We would like to thank nurse Hanne Watts for efficiently enrolling patients in the study, and the radiologist colleges who performed the elastography measurements. Thanks to Karin Larsen from Department of Oncology for professional linguistic assistance. The region of Southern Denmark and the Danish Council of Radiographers supported this study.

Conflicts of Interest

The authors declare that they have no conflict of interest.

References


